

# Endoscopic navigation in the absence of CT imaging

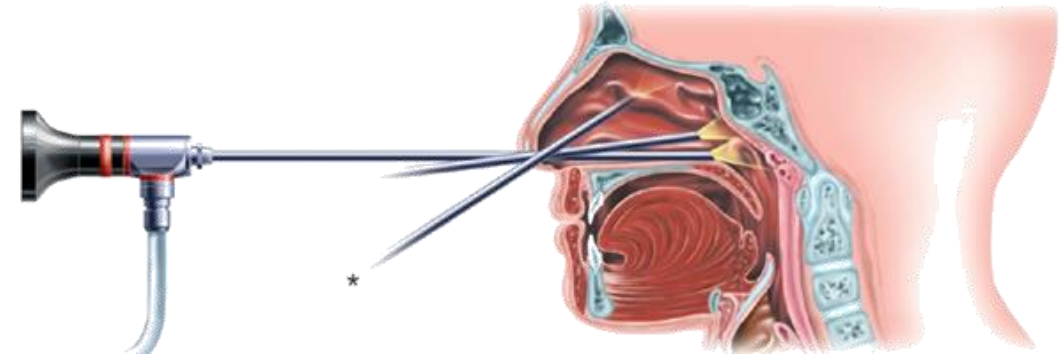
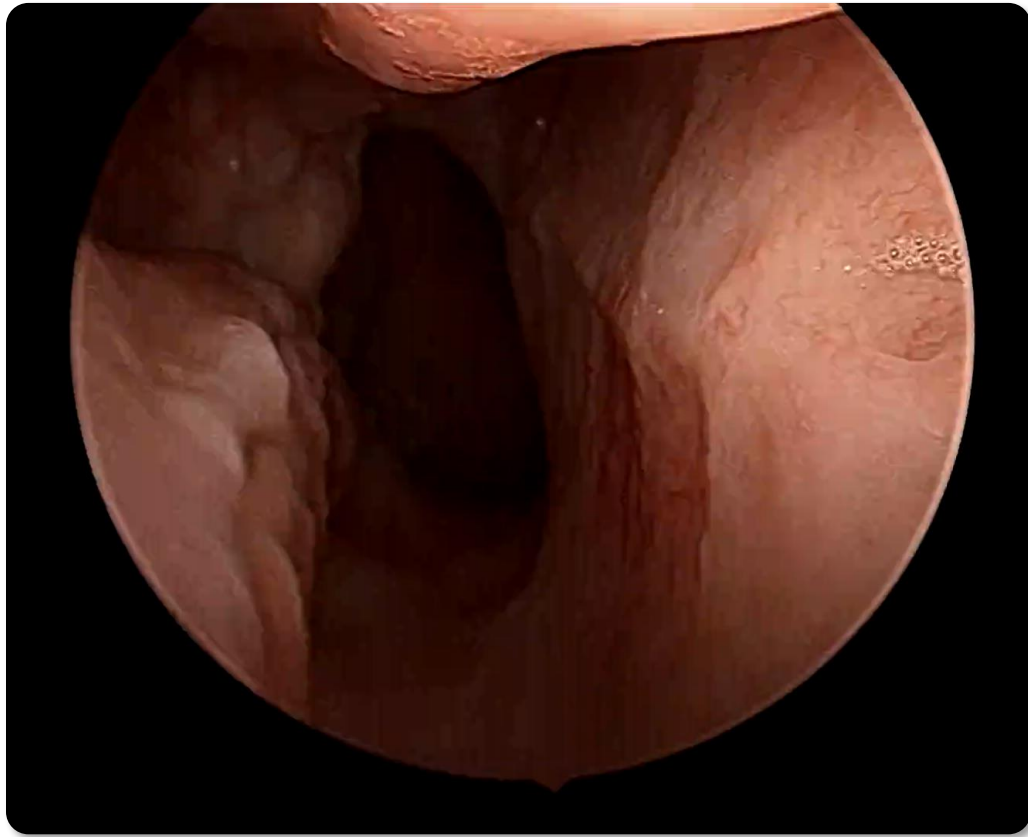
Ayushi Sinha<sup>1,✉</sup>, Xingtong Liu<sup>1</sup>, Austin Reiter<sup>1</sup>, Masaru Ishii<sup>2</sup>,  
Greg Hager<sup>1</sup>, Russ Taylor<sup>1</sup>

<sup>1</sup>The Johns Hopkins University, Baltimore, USA

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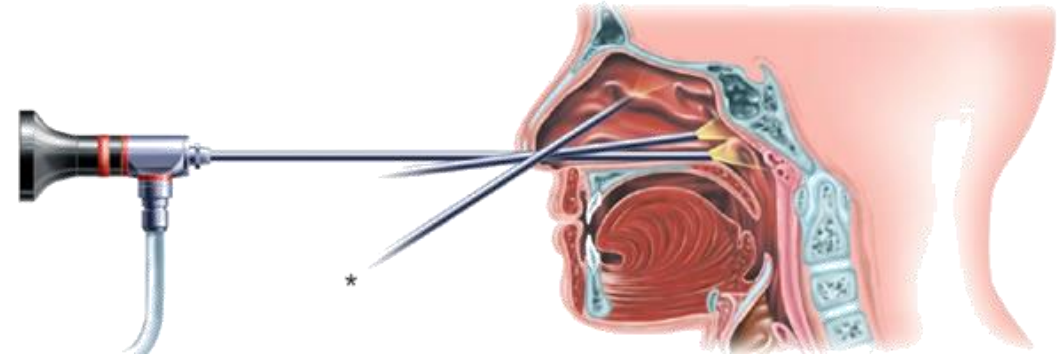
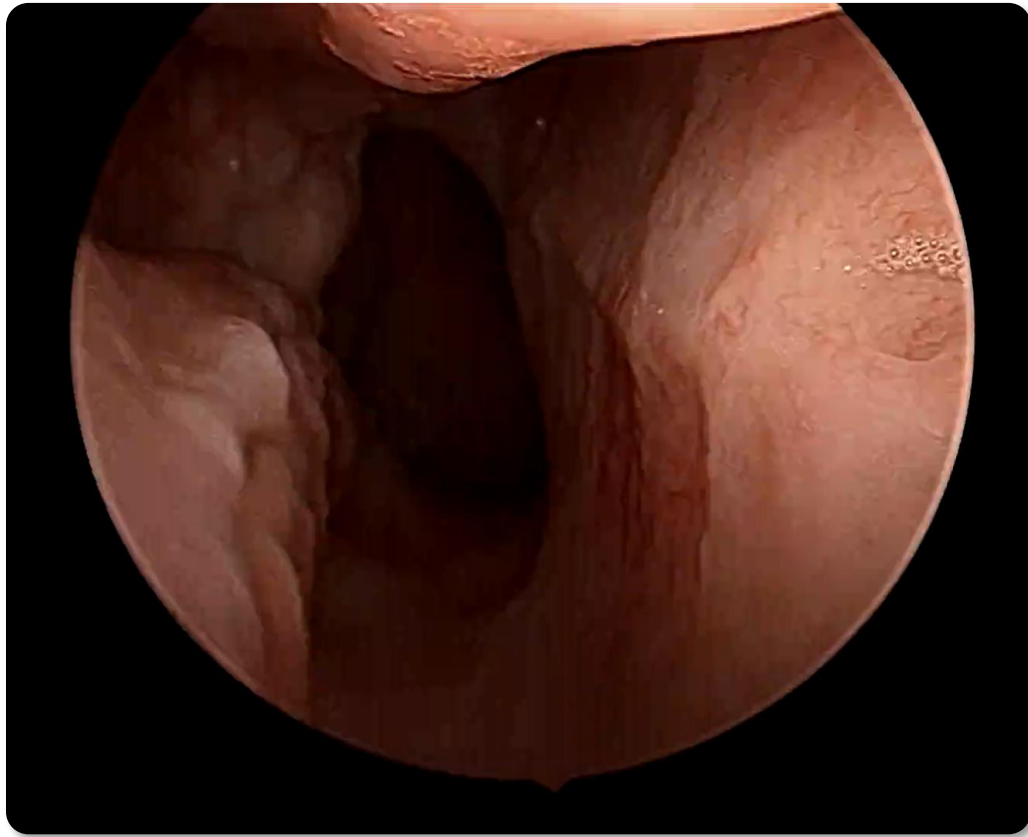
Code: <https://github.com/AyushiSinha/cisstICP>  
✉ [sinha@jhu.edu](mailto:sinha@jhu.edu)

# Nasal endoscopy in the clinic



G. Scadding et al., *Diagnostic tools in Rhinology EAACI position paper*, Clinical and Translational Allergy, 1(2), 2011

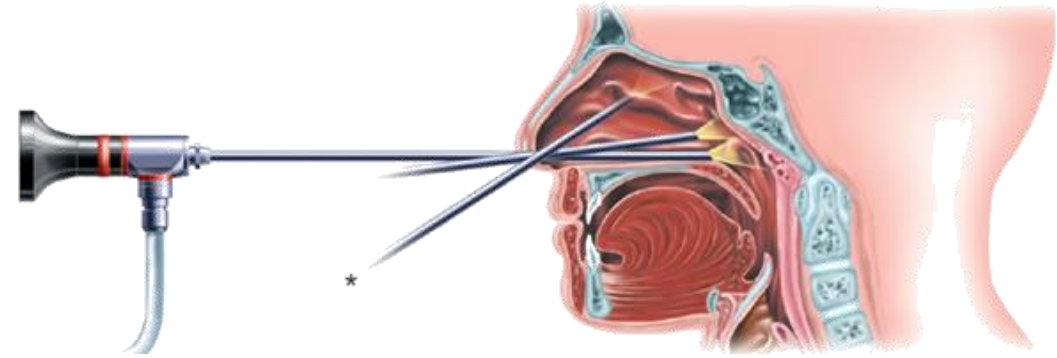
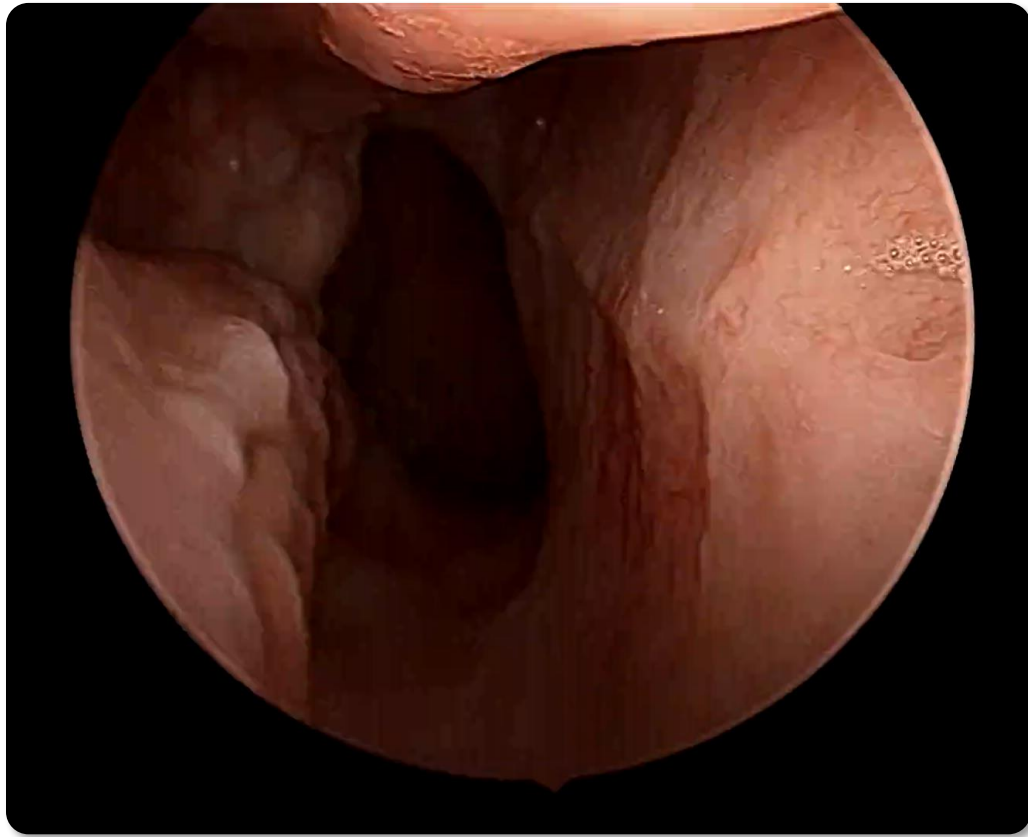
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Navigation without additional tools

# Nasal endoscopy in the clinic

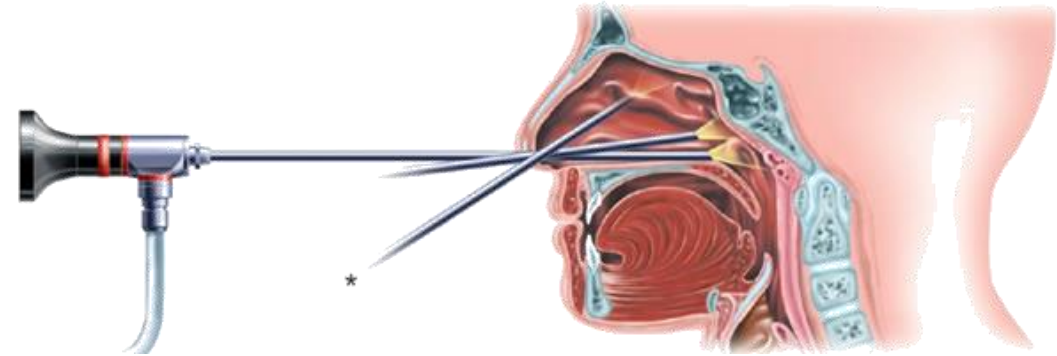
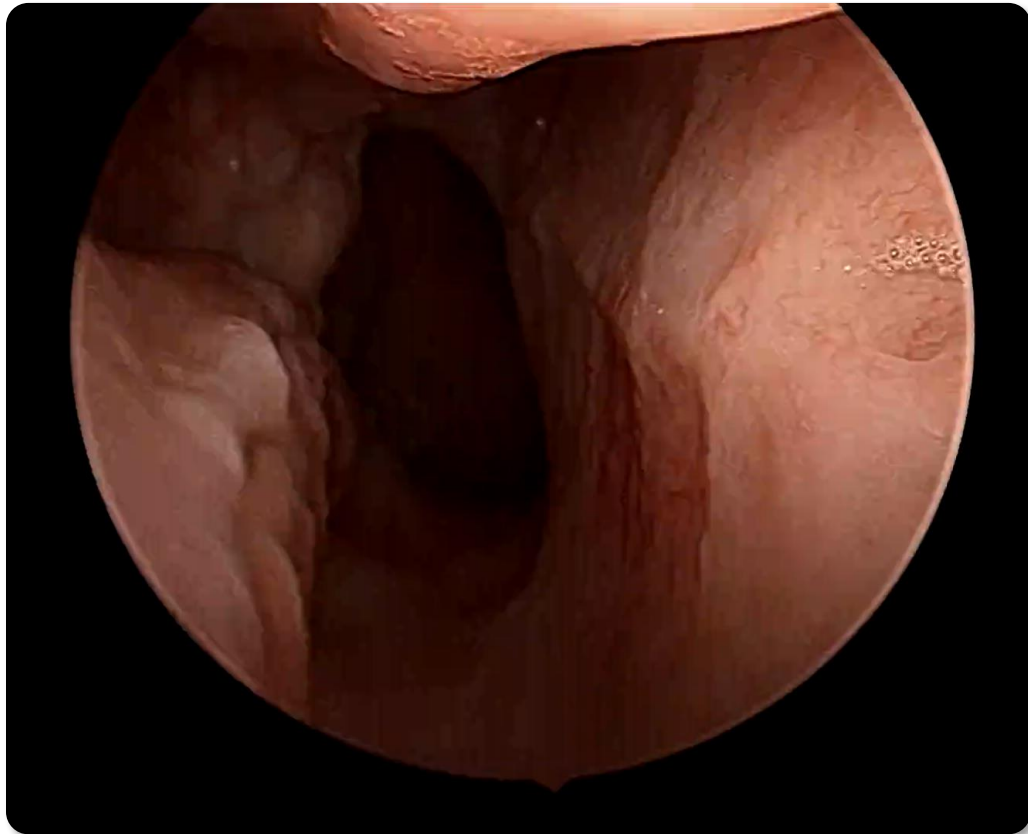


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Navigation without additional tools

Estimate anatomy without CT scan

# Nasal endoscopy in the clinic



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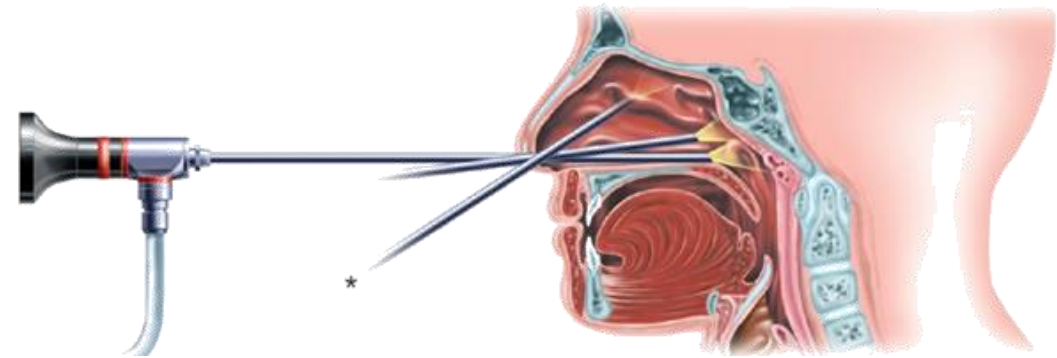
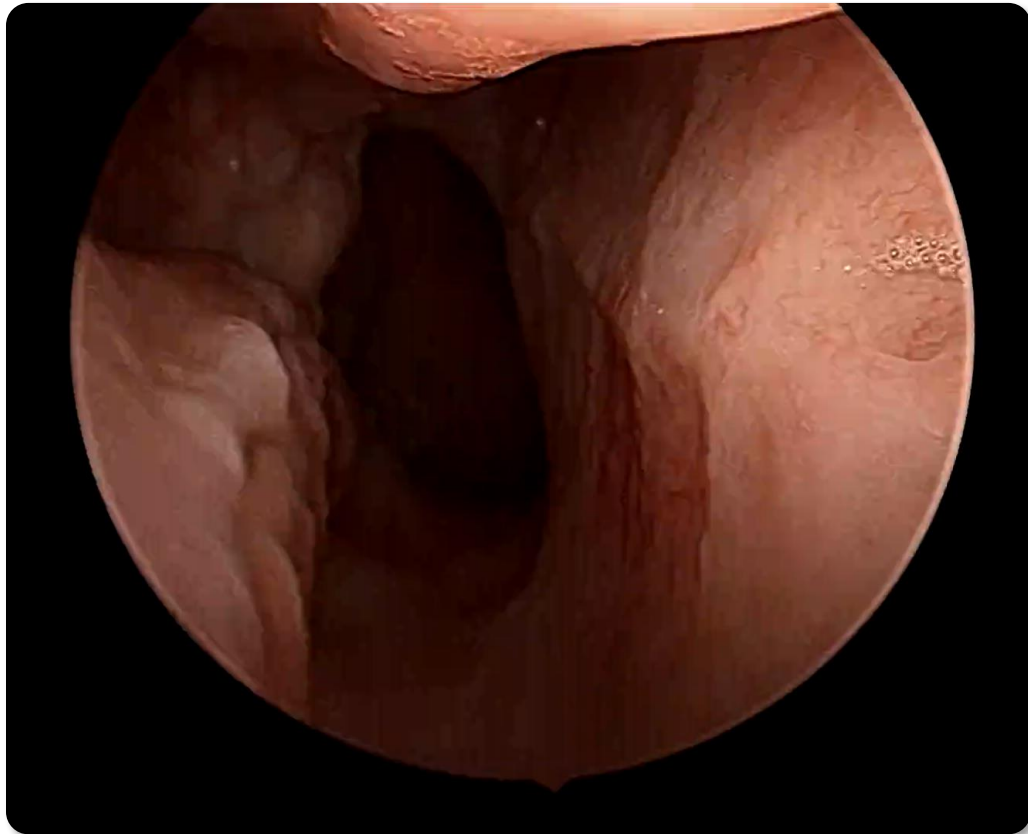
Navigation without additional tools

Estimate anatomy without CT scan

Assign confidence to registration



# Nasal endoscopy in the clinic



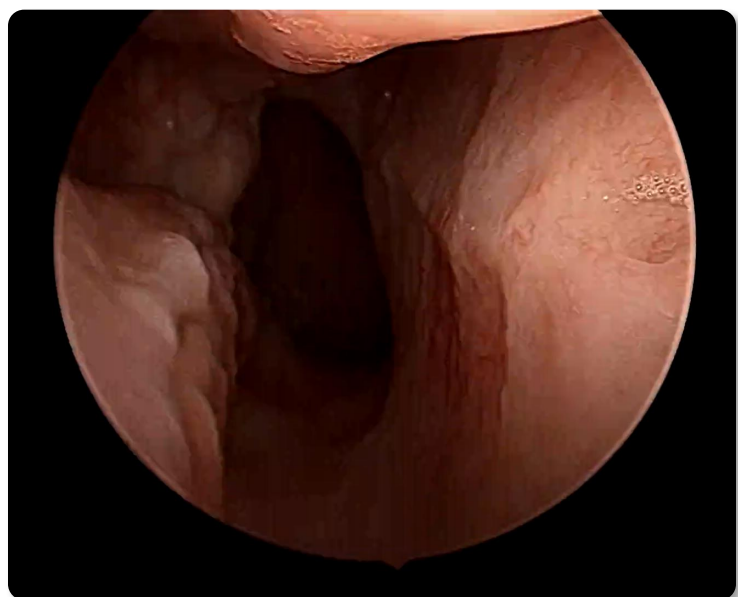
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Navigation without additional tools

Estimate anatomy without CT scan

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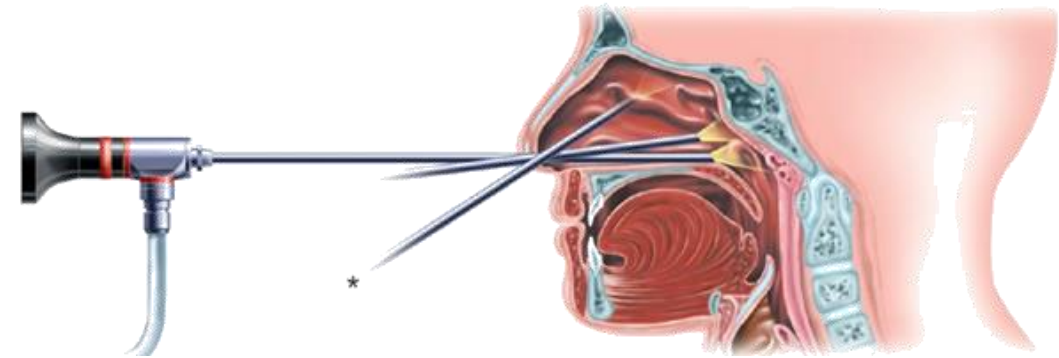
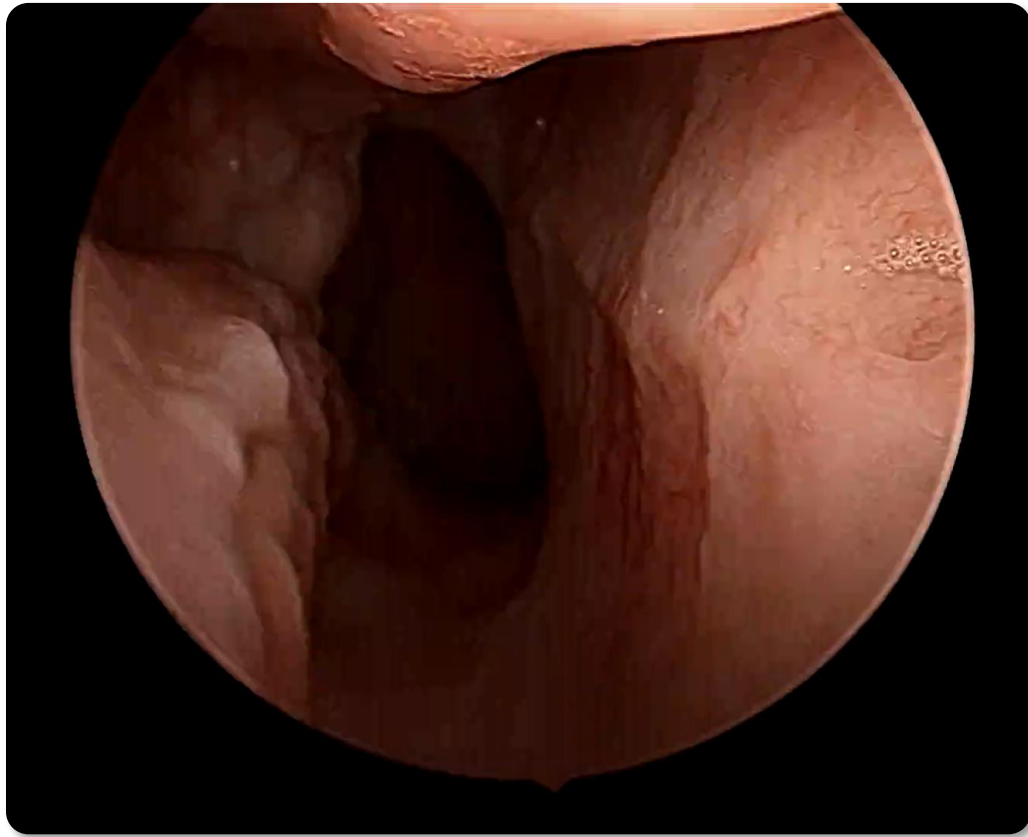
# Navigation without additional tools



Learning-based  
method



# Nasal endoscopy in the clinic



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Navigation without additional tools

Estimate anatomy without CT scan

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# Estimate anatomy without CT scan

- Build statistical shape models
  - Principal component analysis
  - Capture anatomical variation
- Deformable registration
  - Optimize PCA model parameters
  - Produce registration score

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# Statistical shape models

- Given shapes,  $\mathbf{V} = [\mathbf{v}_1 \ \mathbf{v}_2 \ \dots \ \mathbf{v}_{n_v}]^{\mathbf{T}}$ , with correspondences, we can compute:

- Mean:

$$\bar{\mathbf{V}} = \frac{1}{n_s} \sum_{i=1}^{n_s} \mathbf{V}_i$$

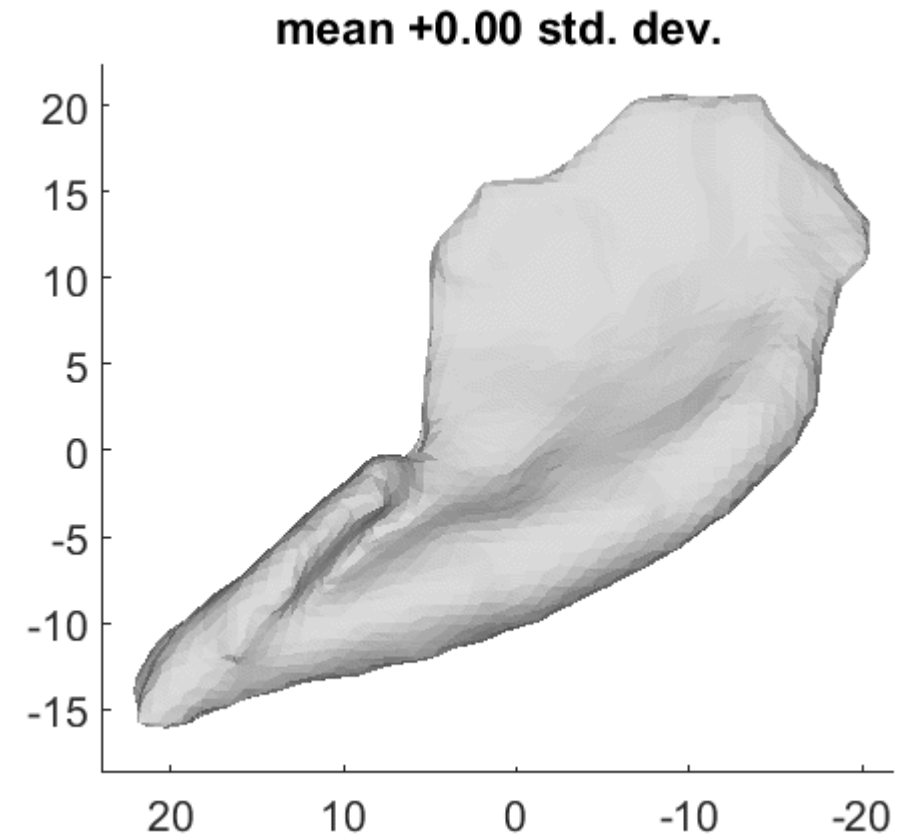
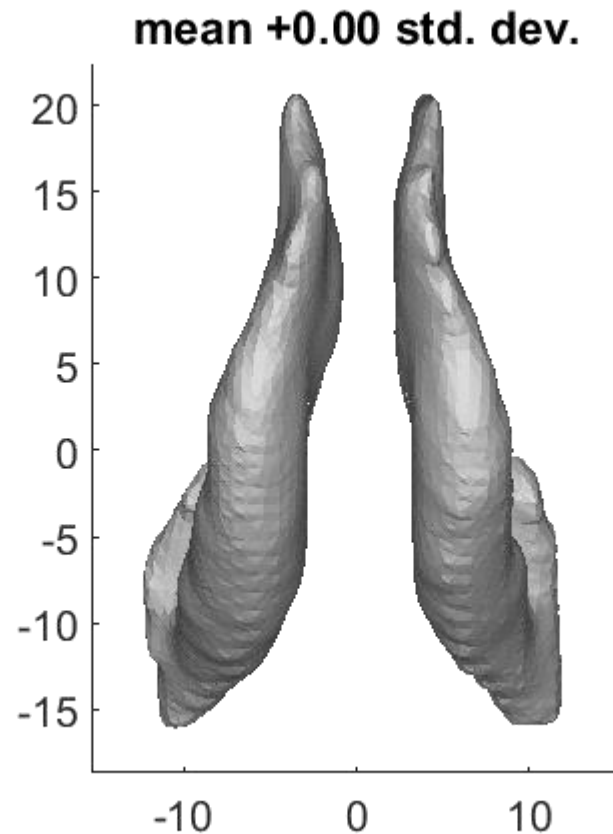
- Variance:

$$\Sigma = \frac{1}{n_s} \sum_{i=1}^{n_s} (\mathbf{V}_i - \bar{\mathbf{V}})(\mathbf{V}_i - \bar{\mathbf{V}})^{\mathbf{T}}$$

$$\Sigma = [\mathbf{m}_1 \ \dots \ \mathbf{m}_{n_s}] \begin{bmatrix} \lambda_1 & & \\ & \ddots & \\ & & \lambda_{n_s} \end{bmatrix} [\mathbf{m}_1 \ \dots \ \mathbf{m}_{n_s}]^{\mathbf{T}}$$

# Statistical shape models

- Variance along the principal mode for middle turbinates



# Statistical shape models

- Given a new shape,  $\mathbf{V}^*$ , we can compute:

- Mode weights:

$$s_i = \mathbf{w}_i^T (\mathbf{V}^* - \bar{\mathbf{V}})$$

$$\mathbf{w}_i = \sqrt{\lambda_i} \mathbf{m}_i$$

- Estimated shape:

$$\tilde{\mathbf{V}}^* = \bar{\mathbf{V}} + \sum_{i=1}^{n_m} s_i \mathbf{w}_i$$



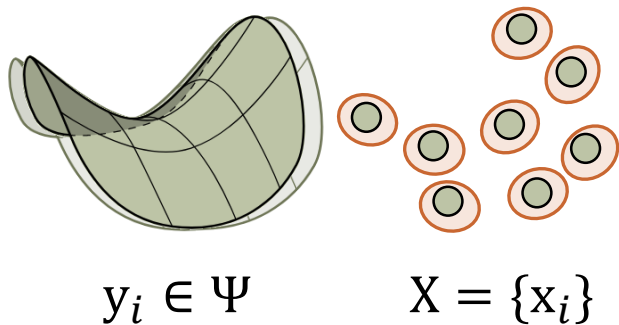
# Estimate anatomy without CT scan

- Build statistical shape models
  - Principal component analysis
  - Capture anatomical variation
- Deformable registration
  - Optimize PCA model parameters
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# Deformable most likely point (D-IMLP)

$$T = \operatorname{argmin}_{[a, \mathbf{R}, \mathbf{t}], s} \left( \frac{1}{2} \sum_{i=1}^{n_{\text{data}}} \left( (T_{\text{ssm}}(\mathbf{y}_i) - a\mathbf{R}\mathbf{x}_i - \mathbf{t})^T (\mathbf{R}\Sigma_{\mathbf{x}_i}\mathbf{R}^T)^{-1} (T_{\text{ssm}}(\mathbf{y}_i) - a\mathbf{R}\mathbf{x}_i - \mathbf{t}) \right) \right)$$

Find  $\mathbf{R}$ ,  $\mathbf{t}$  and  $a$  such that  $\mathbf{x}$  is best aligned with a deformed  $\mathbf{y}$ ...



$$+ \frac{1}{2} \sum_{j=1}^{n_m} \|s_j\|_2^2 \right)$$

Find  $s$  such that  $\mathbf{y}$  deforms to fit  $\mathbf{x}$

$$T_{\text{ssm}}(\mathbf{y}_i) = f(\mathbf{y}_i, s)$$

# Generalized deformable most likely oriented point (GD-IMLOP)

$$T = \operatorname{argmin}_{[a, \mathbf{R}, \mathbf{t}], s} \left( \frac{1}{2} \sum_{i=1}^{n_{\text{data}}} \left( (T_{\text{ssm}}(\mathbf{y}_i) - a\mathbf{R}\mathbf{x}_i - \mathbf{t})^T (\mathbf{R}\Sigma_{\mathbf{x}_i}\mathbf{R}^T)^{-1} (T_{\text{ssm}}(\mathbf{y}_i) - a\mathbf{R}\mathbf{x}_i - \mathbf{t}) \right) \right)$$

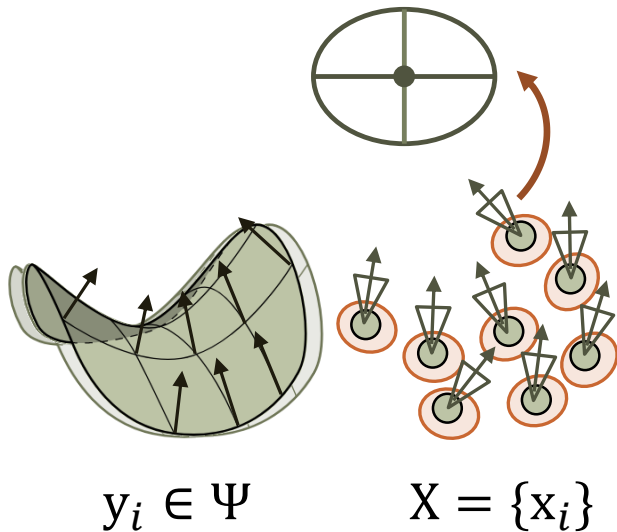
Find  $\mathbf{R}$ ,  $\mathbf{t}$  and  $a$  such that  $\mathbf{x}$  is best aligned with a deformed  $\mathbf{y}$ ...

$$- \sum_{i=1}^{n_{\text{data}}} \left( \kappa_i \hat{\mathbf{y}}_{\mathbf{n}_i} \mathbf{R} \hat{\mathbf{x}}_{\mathbf{n}_i} + \beta_i \left( (\hat{\gamma}_{1_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i})^2 - (\hat{\gamma}_{2_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i})^2 \right) \right)$$

and such that the normal of  $\mathbf{y}$  aligns with that of  $\mathbf{x}$

$$+ \frac{1}{2} \sum_{j=1}^{n_{\text{m}}} \|s_j\|_2^2$$

Find  $s$  such that  $\mathbf{y}$  deforms to fit  $\mathbf{x}$

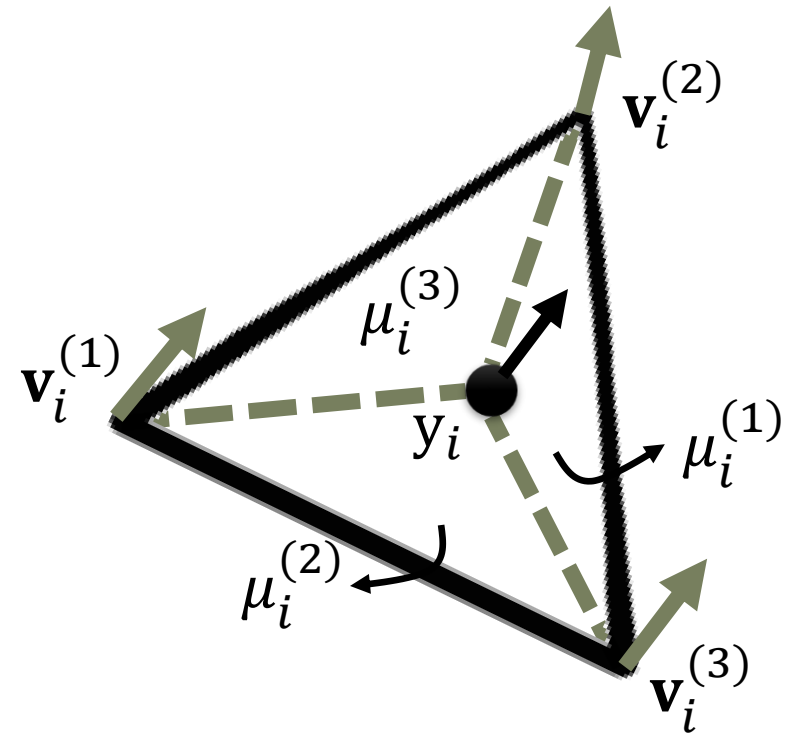


$$T_{\text{ssm}}(\mathbf{y}_i) = f(\mathbf{y}_i, s), \quad \kappa_0 = \frac{1}{\sigma_{\text{circ\_rad}}^2}, \quad \beta = e^{\frac{\kappa}{2}}$$

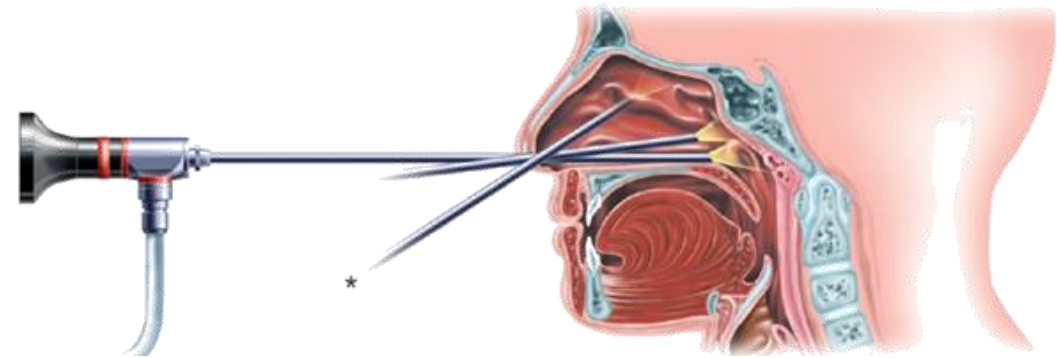
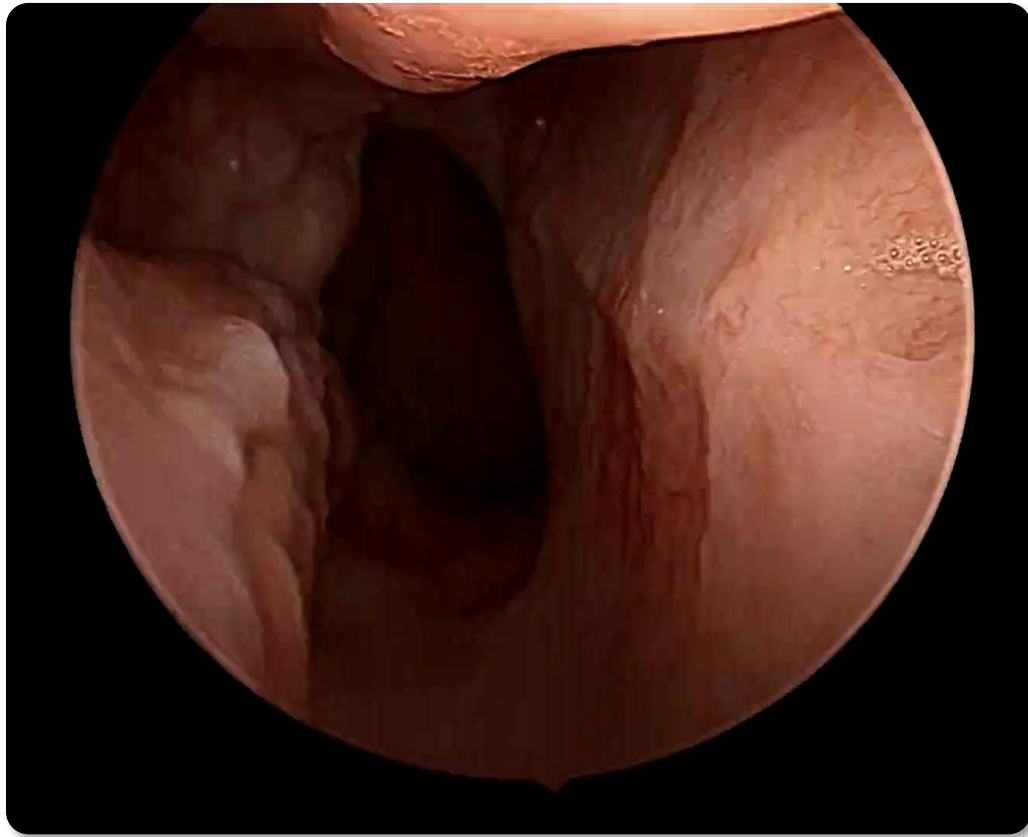
What is  $T_{\text{ssm}}(\mathbf{y}_i)$ ?

$$T_{\text{ssm}}(\mathbf{v}_i) = \bar{\mathbf{v}}_i + \sum_{j=1}^{n_{\mathbf{m}}} s_j \mathbf{w}_j^{(i)}$$

$$T_{\text{ssm}}(\mathbf{y}_i) = \sum_{j=1}^3 \mu_i^{(j)} T_{\text{ssm}}(\mathbf{v}_i^{(j)})$$
$$\sum_{j=1}^3 \mu_i^{(j)} = 1$$



# Nasal endoscopy in the clinic



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Navigation without additional tools

Estimate anatomy without CT scan

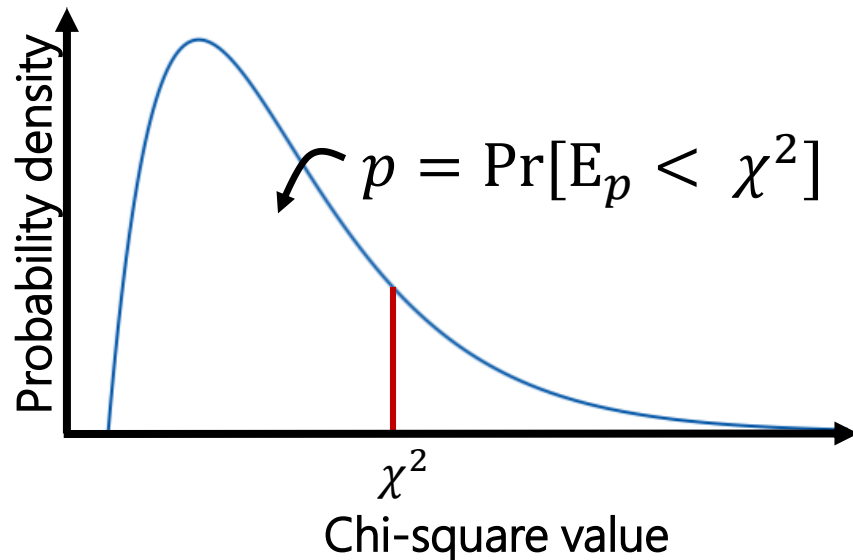
Assign confidence to registration



# Did it work?

$$E_p = \sum_{i=1}^{n_{\text{data}}} \left( (T_{\text{ssm}}(\mathbf{y}_i) - a\mathbf{R}\mathbf{x}_i - \mathbf{t})^T (\mathbf{R}\Sigma_{\mathbf{x}_i}\mathbf{R}^T)^{-1} (T_{\text{ssm}}(\mathbf{y}_i) - a\mathbf{R}\mathbf{x}_i - \mathbf{t}) \right) \approx \chi^2 \text{ distribution}$$

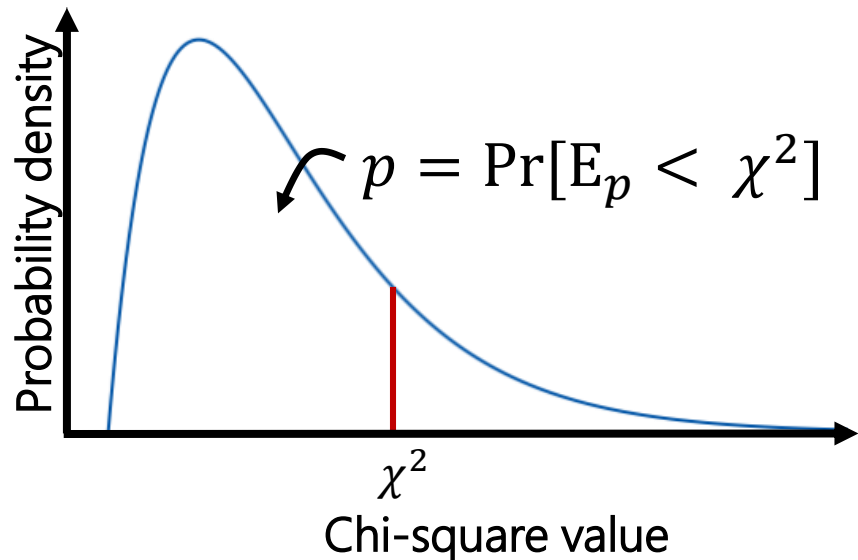
$$E_o = \sum_{i=1}^{n_{\text{data}}} \begin{bmatrix} \cos^{-1}(\hat{\mathbf{y}}_{\mathbf{n}_i}^T \mathbf{R} \hat{\mathbf{x}}_{\mathbf{n}_i}) \\ \sin^{-1}(\hat{\gamma}_{1_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i}) \\ \sin^{-1}(\hat{\gamma}_{2_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i}) \end{bmatrix}^T \begin{bmatrix} \kappa_i & 0 & 0 \\ 0 & \kappa_i - 2\beta_i & 0 \\ 0 & 0 & \kappa_i + 2\beta_i \end{bmatrix} \begin{bmatrix} \cos^{-1}(\hat{\mathbf{y}}_{\mathbf{n}_i}^T \mathbf{R} \hat{\mathbf{x}}_{\mathbf{n}_i}) \\ \sin^{-1}(\hat{\gamma}_{1_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i}) \\ \sin^{-1}(\hat{\gamma}_{2_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i}) \end{bmatrix} \approx \chi^2 \text{ distribution}$$



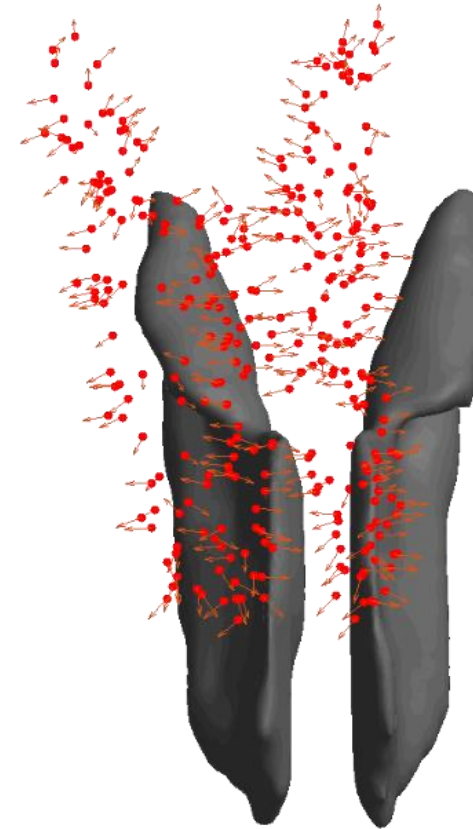
# Did it work?

$$E_p = \sum_{i=1}^{n_{\text{data}}} \left( (T_{\text{ssm}}(\mathbf{y}_i) - a\mathbf{R}\mathbf{x}_i - \mathbf{t})^T (\mathbf{R}\Sigma_{\mathbf{x}_i}\mathbf{R}^T)^{-1} (T_{\text{ssm}}(\mathbf{y}_i) - a\mathbf{R}\mathbf{x}_i - \mathbf{t}) \right) \leq \text{chi2inv}(p, 3n_{\text{data}})$$

$$E_o = \sum_{i=1}^{n_{\text{data}}} \begin{bmatrix} \cos^{-1}(\hat{\mathbf{y}}_{\mathbf{n}_i}^T \mathbf{R} \hat{\mathbf{x}}_{\mathbf{n}_i}) \\ \sin^{-1}(\hat{\gamma}_{1_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i}) \\ \sin^{-1}(\hat{\gamma}_{2_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i}) \end{bmatrix}^T \begin{bmatrix} \kappa_i & 0 & 0 \\ 0 & \kappa_i - 2\beta_i & 0 \\ 0 & 0 & \kappa_i + 2\beta_i \end{bmatrix} \begin{bmatrix} \cos^{-1}(\hat{\mathbf{y}}_{\mathbf{n}_i}^T \mathbf{R} \hat{\mathbf{x}}_{\mathbf{n}_i}) \\ \sin^{-1}(\hat{\gamma}_{1_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i}) \\ \sin^{-1}(\hat{\gamma}_{2_i}^T \mathbf{R}^T \hat{\mathbf{y}}_{\mathbf{n}_i}) \end{bmatrix} \leq \text{chi2inv}(p, 2n_{\text{data}})$$



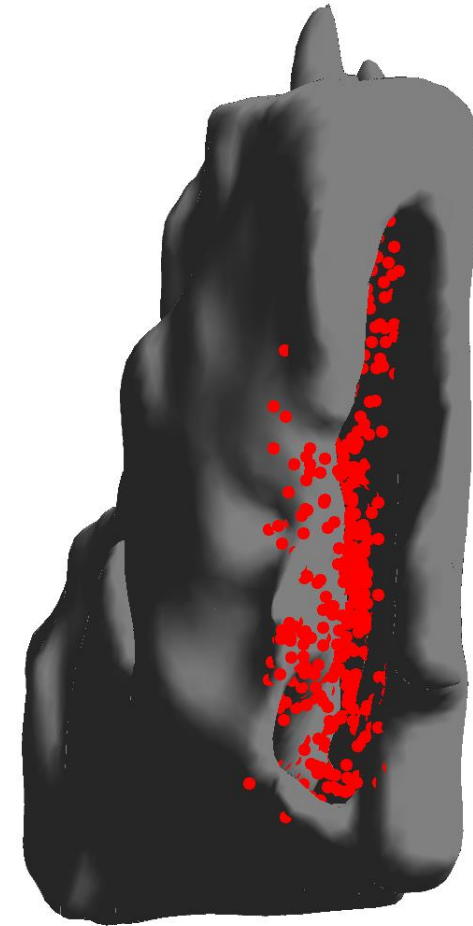
GD-IMLOP Iteration: 1



# Experiments

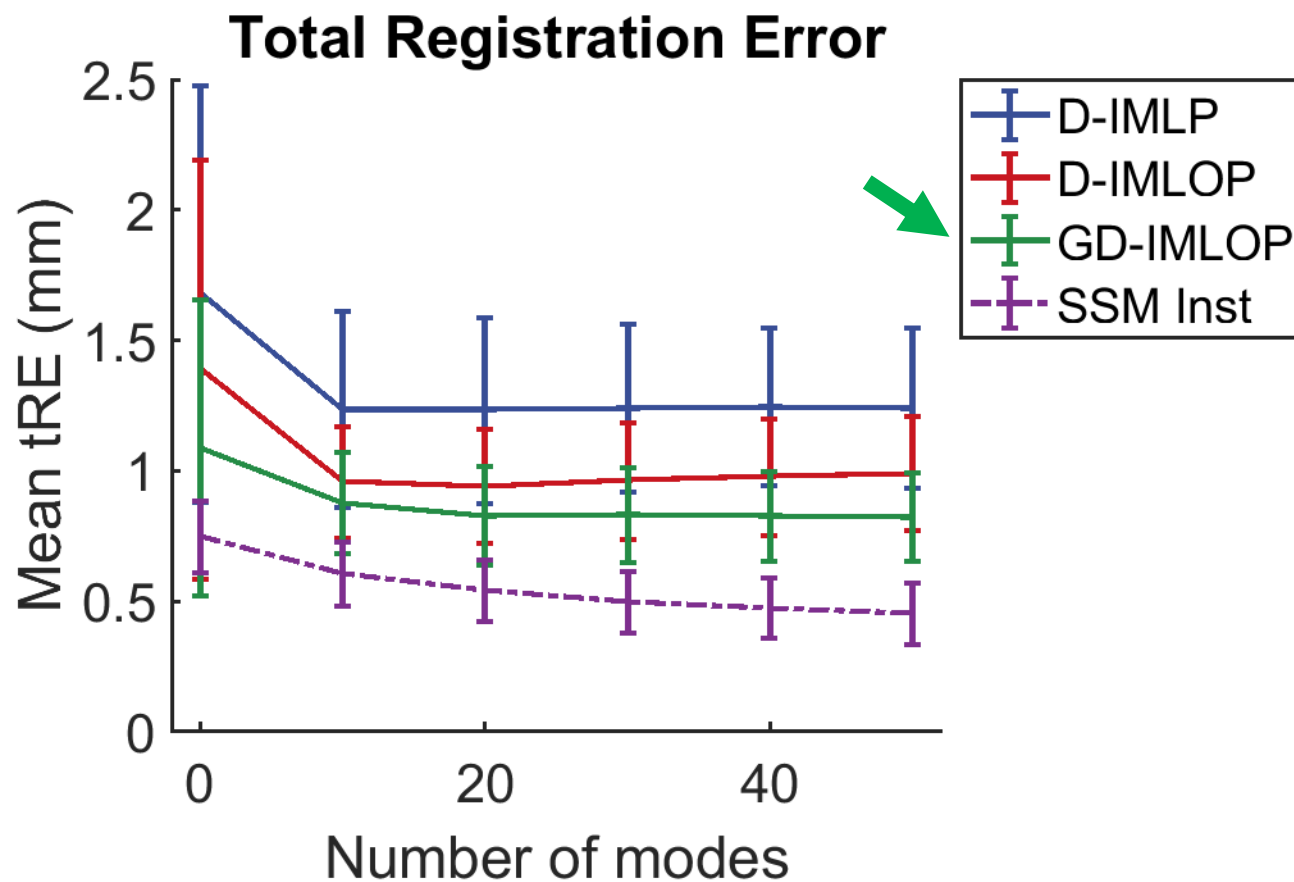
# Leave-one-out

- # sample point: 3000
- Translational offset:  $[0, 10]$  mm
- Rotational offset:  $[0, 10]$  degrees
- Noise:
  - $0.5 \times 0.5 \times 0.75 \text{mm}^3$
  - $10^\circ$  ( $e = 0.5$ )
- Noise assumed:
  - $1 \times 1 \times 2 \text{mm}^3$
  - $30^\circ$  ( $e = 0.5$ )
- $n_m \in \{0, 10, 20, 30, 40, 50\}$

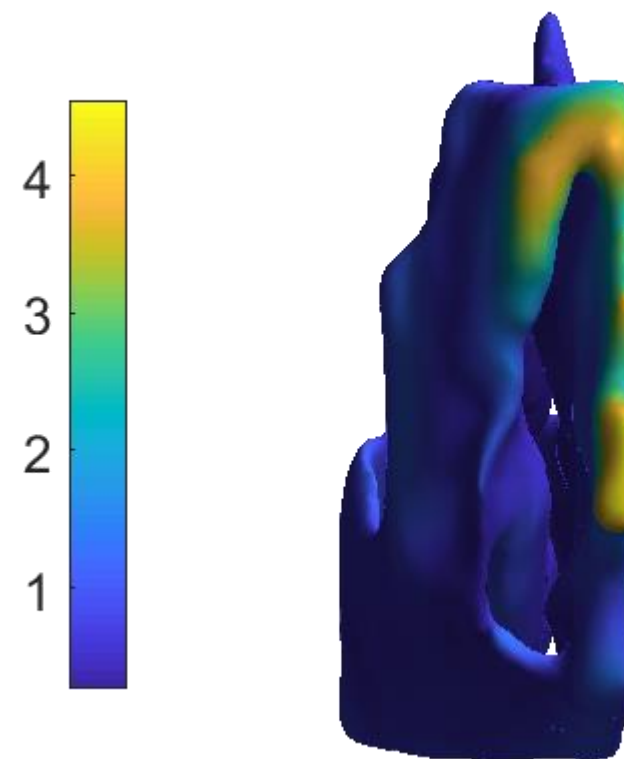


Right nasal airway

# Leave-one-out



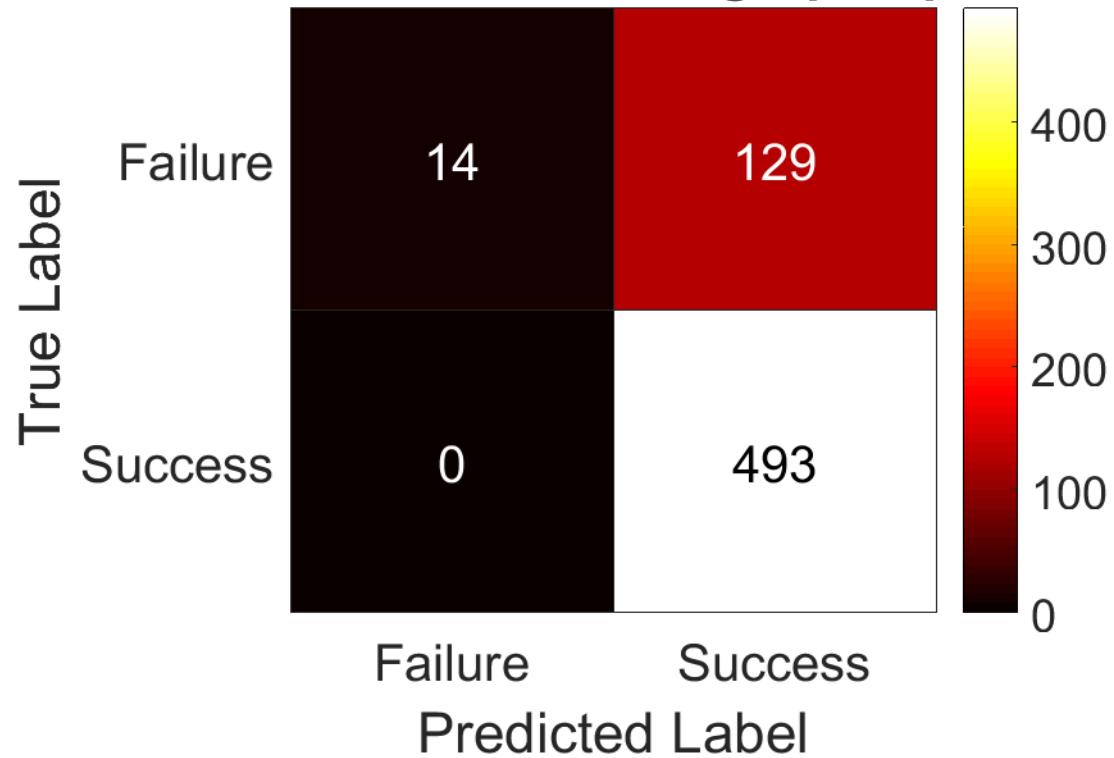
### Shape estimation error (50 modes)



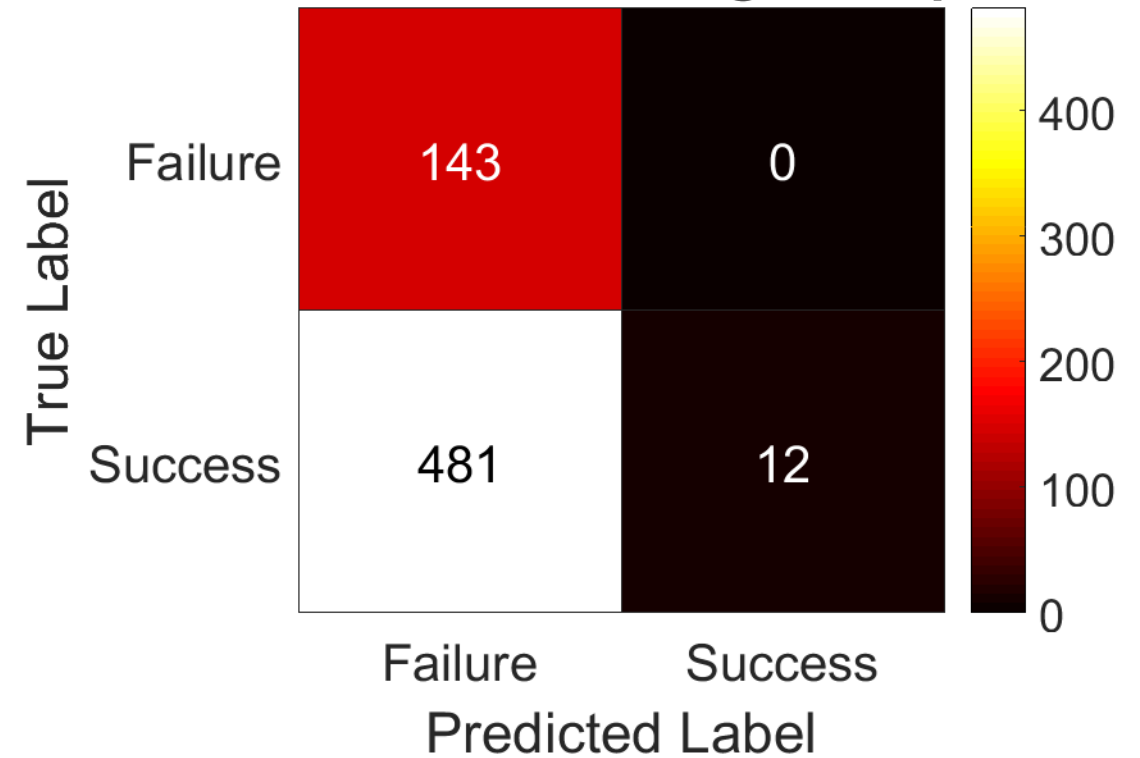


# Leave-one-out

**Confusion Matrix using Ep at  $p=0.95$**

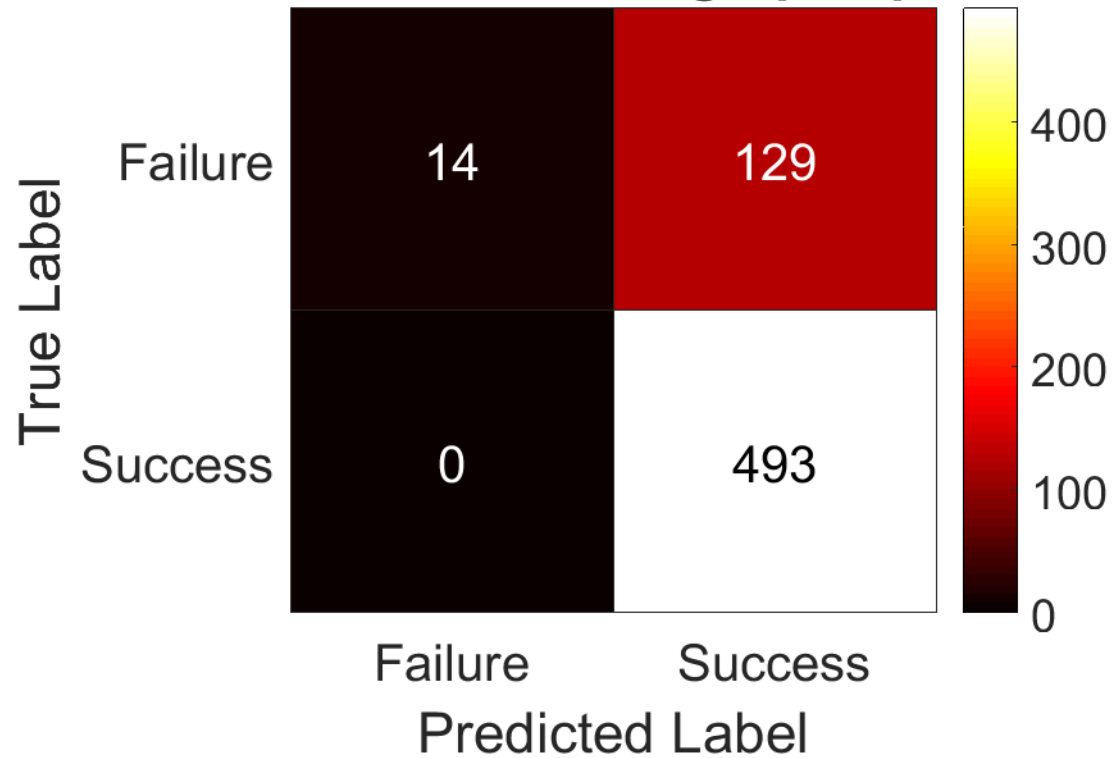


**Confusion Matrix using Eo at  $p=0.95$**

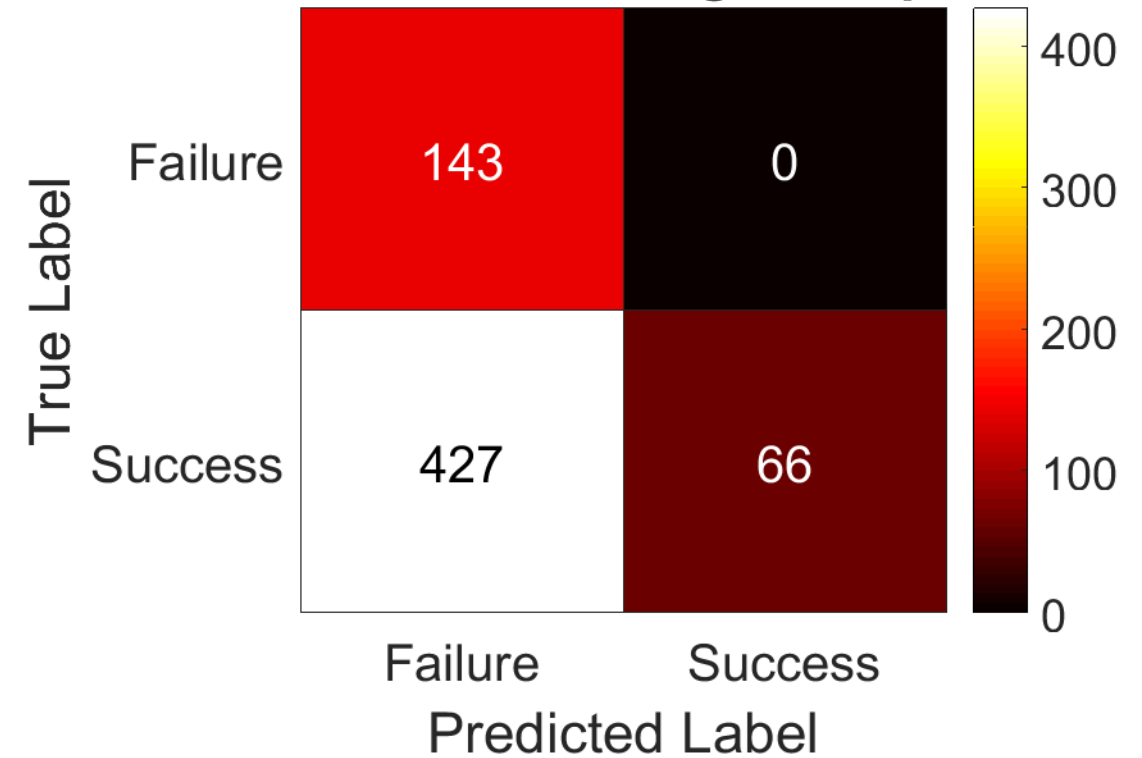


# Leave-one-out

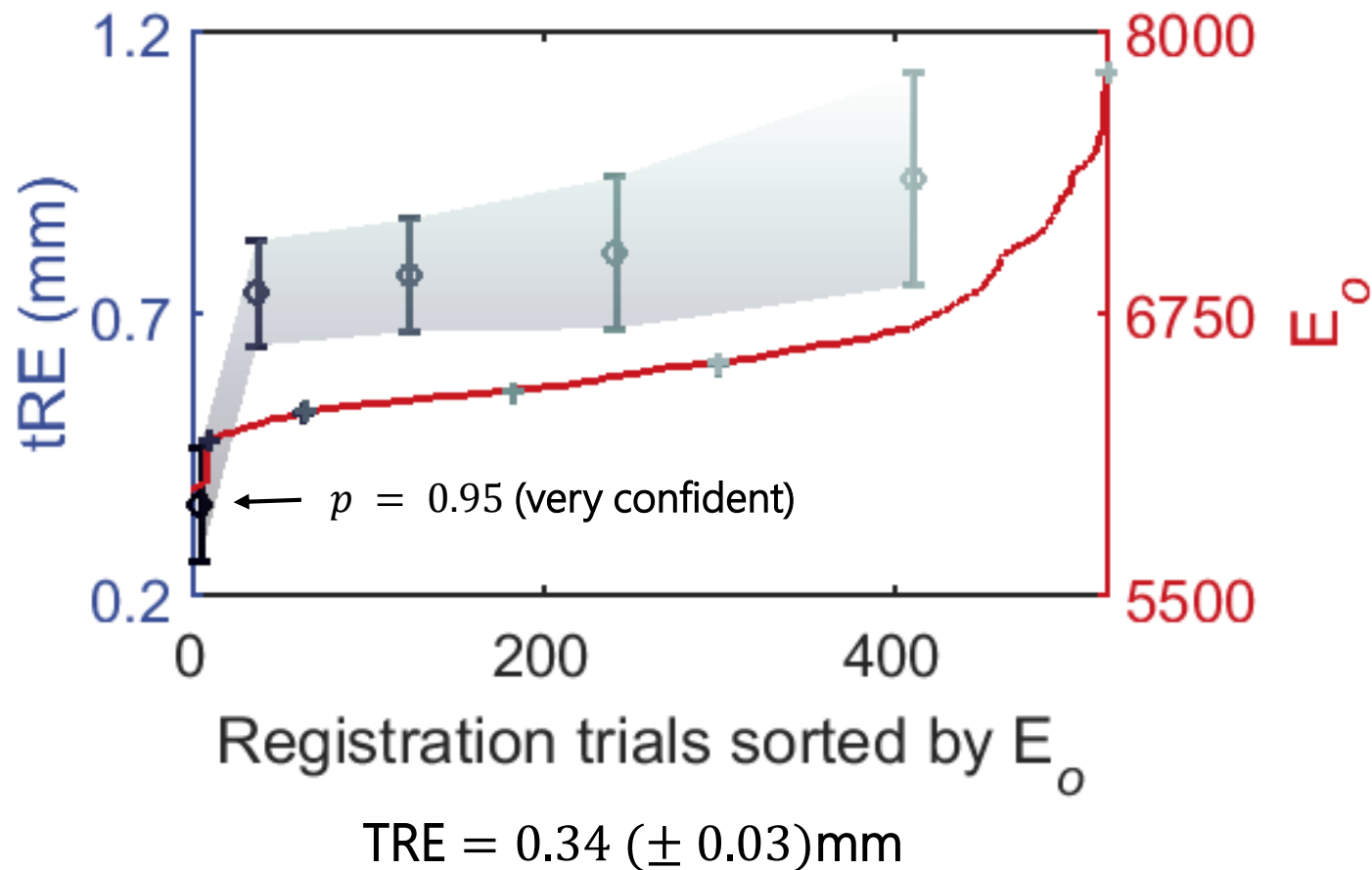
**Confusion Matrix using Ep at  $p=0.9975$**



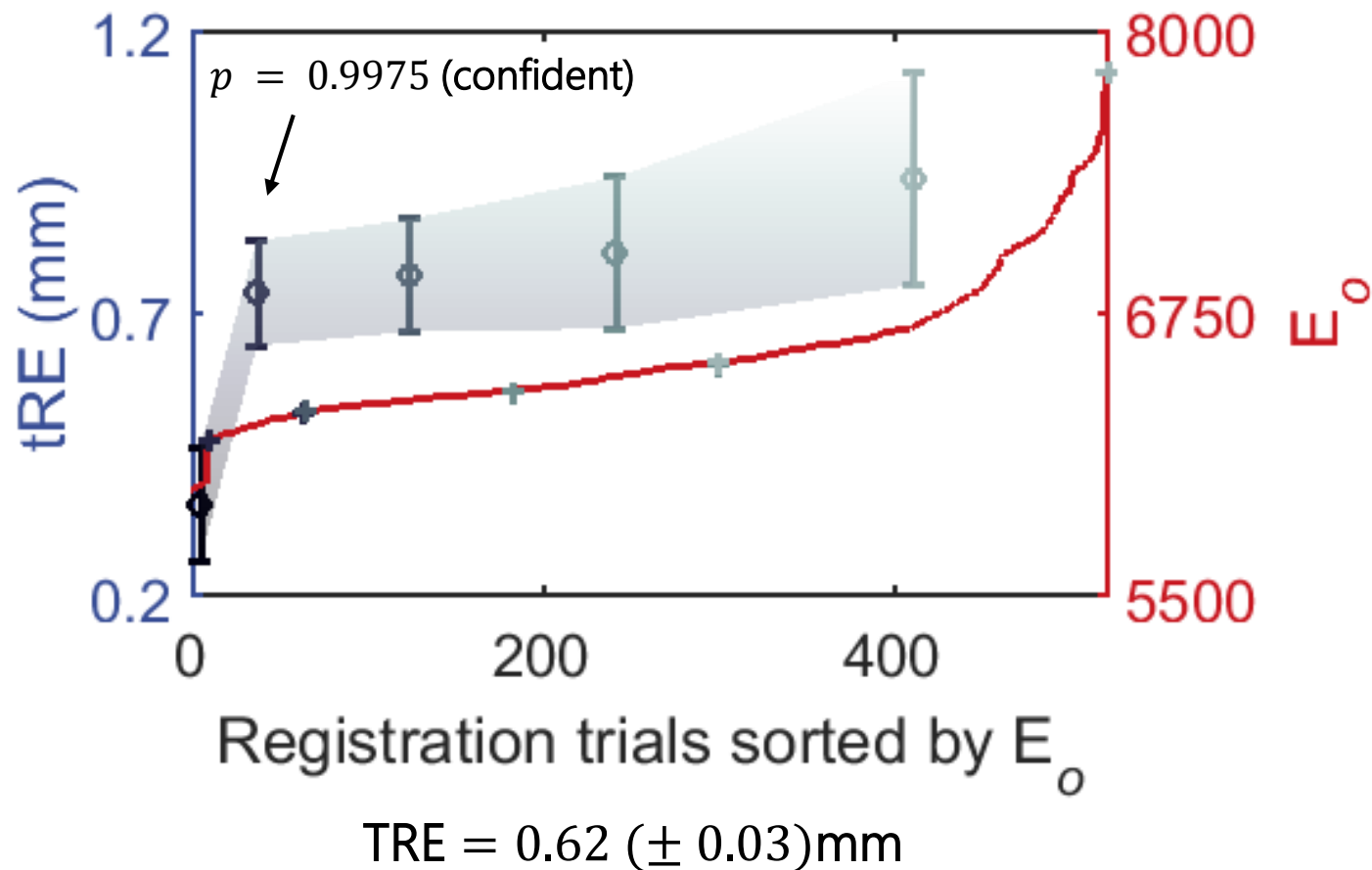
**Confusion Matrix using Eo at  $p=0.9975$**



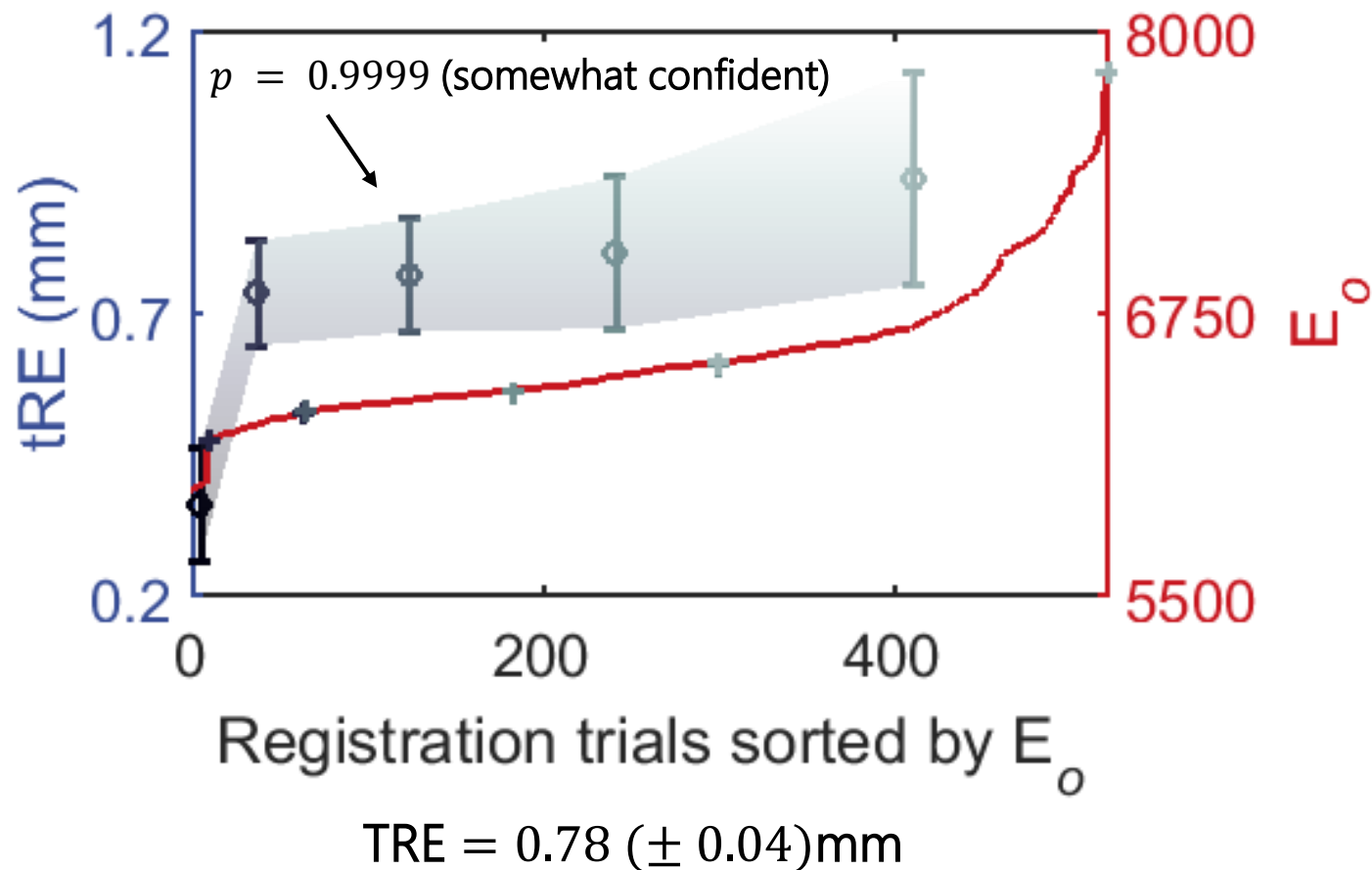
## Decreasing confidence in registration accuracy with increasing $p$



## Decreasing confidence in registration accuracy with increasing $p$

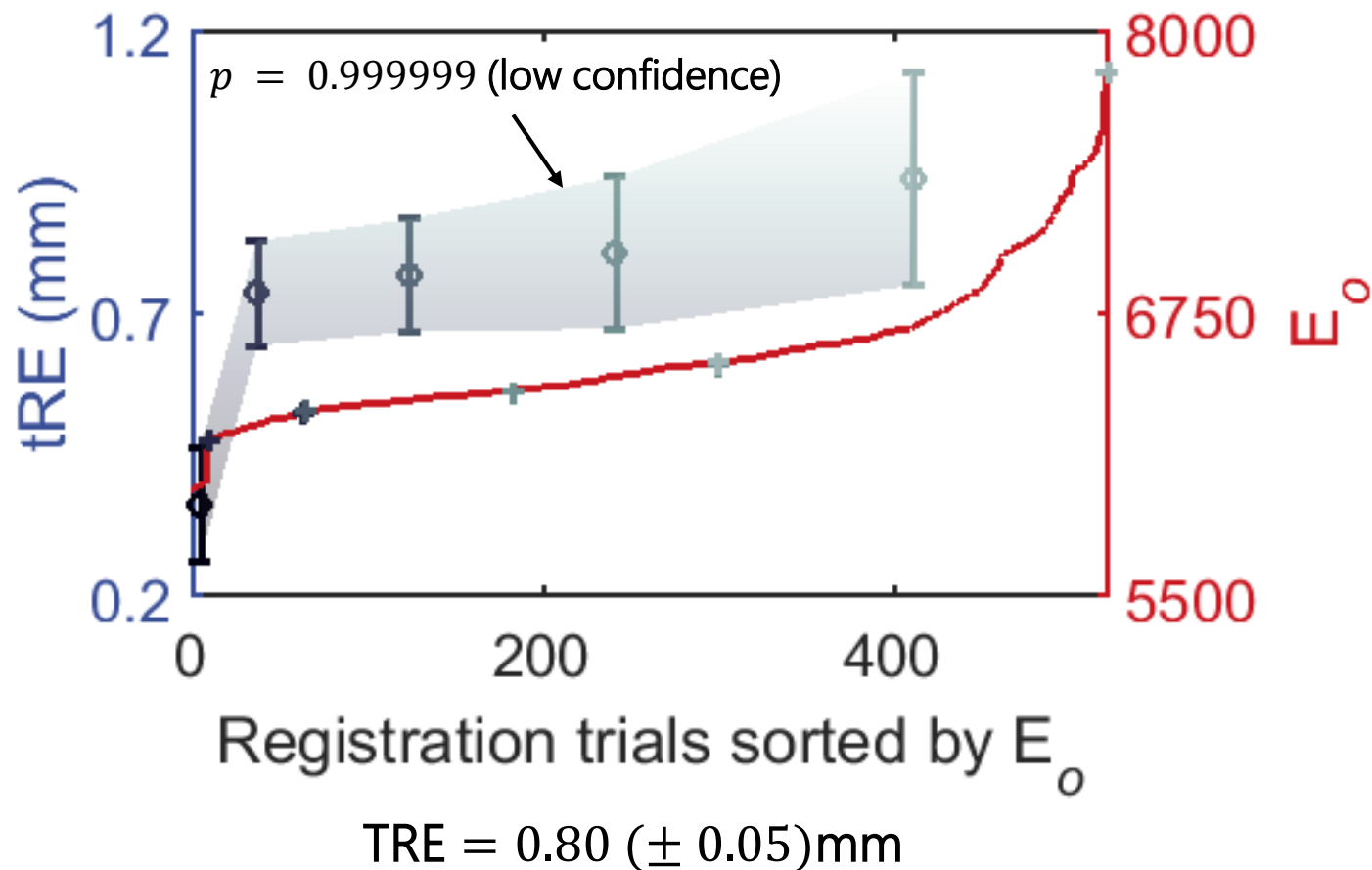


## Decreasing confidence in registration accuracy with increasing $p$

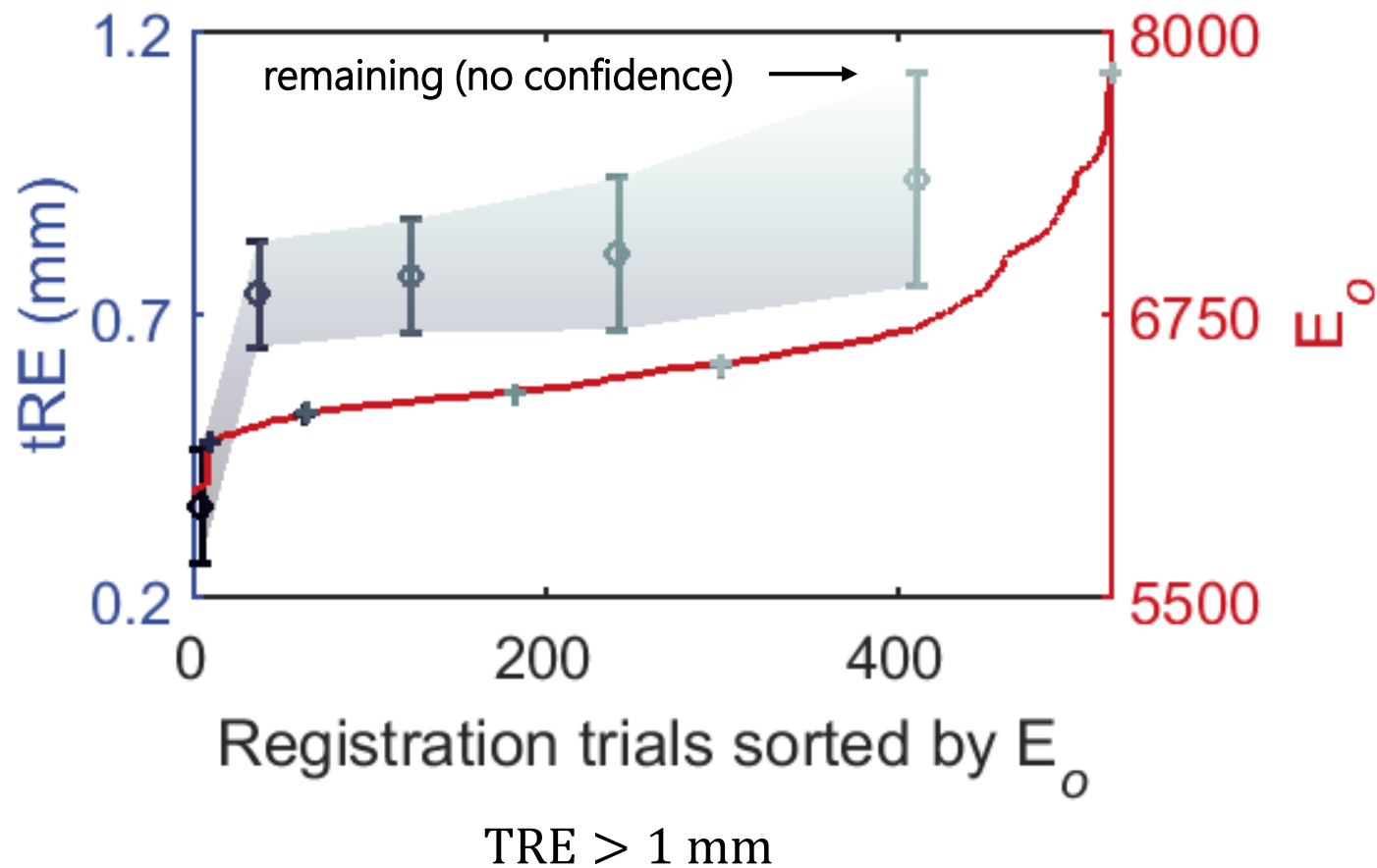




## Decreasing confidence in registration accuracy with increasing $p$



## Decreasing confidence in registration accuracy with increasing $p$



# In vivo

- 5 clinical sequences
- 3000 sample points
- Noise assumed:
  - $1 \times 1 \times 2\text{mm}^3$
  - $30^\circ$  ( $e = 0.5$ )
- $n_{\mathbf{m}} \in \{0, 10, 20, 30, 40, 50\}$

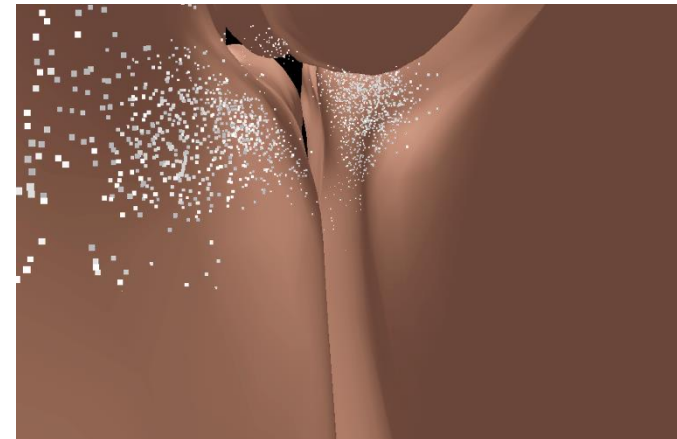
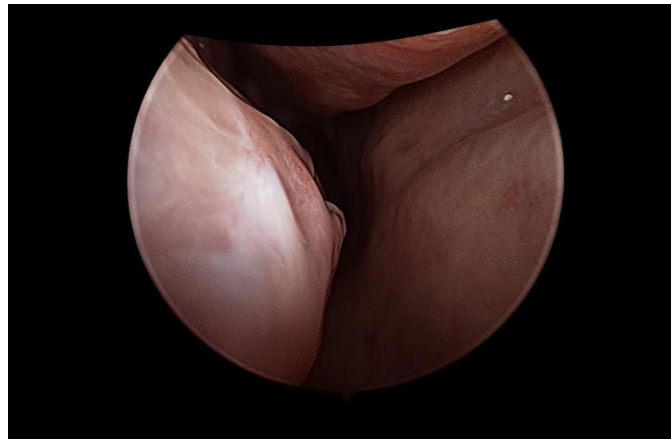


Right nasal airway



Dense reconstruction  
from video

	# registrations	Residual error (mm)	Max error (mm)	Min error (mm)
All registrations	30/30	1.09 ( $\pm 1.03$ )	4.74	0.50
Registrations that pass $E_p$ test	27/30	0.76 ( $\pm 0.14$ )	0.99	0.50
Registrations that pass $E_p$ and $E_o$ tests	12/30	0.78 ( $\pm 0.07$ )	0.94	0.72



# Conclusions and future work

- Navigation without additional tools
- Estimate anatomy without CT scan
- Assign confidence to registration
- Learn statistics from 1000s of CTs
- Use additional features
- Evaluate further on in vivo data



# Thank you!



Code: <https://github.com/AyushiSinha/cisstlCP>

Poster: W-2

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