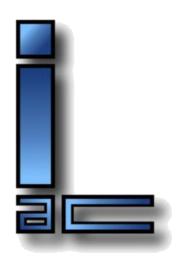
Segmentation-2

Classification, Segmentation, Labeling and Modeling: Modern Approaches

Jerry L. Prince
Image Analysis and Communications
Laboratory
Johns Hopkins University



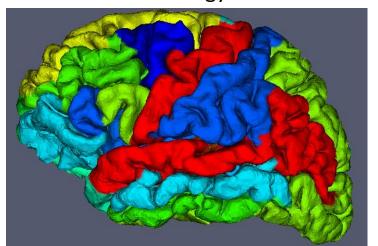
Slide deck structure and many slides taken from Russell H. Taylor "Segmentation and Modeling" slides.



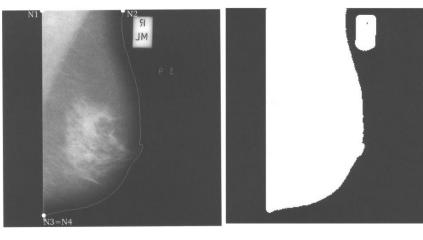
Segmentation Variants

- Image segmentation: divide an image into regions
- Voxel classification: cluster voxel intensities by type
- Voxel labeling: identify voxel anatomy/type by name

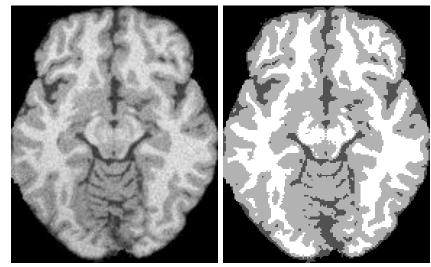
Cortical gyri



Object versus background



Gray matter intensities







Classes of Segmentation Approaches

- Voxel-based versus boundary-based:
 - Voxel-based: voxels are labeled (object vs. background)
 - Boundary-based: boundaries are identified
- Supervised versus unsupervised:
 - Supervised: examples are provided
 - Unsupervised: the data itself provides all information
- Automatic versus semi-automatic
 - Automatic: no user information provided
 - Semi-automatic: some user information is provided

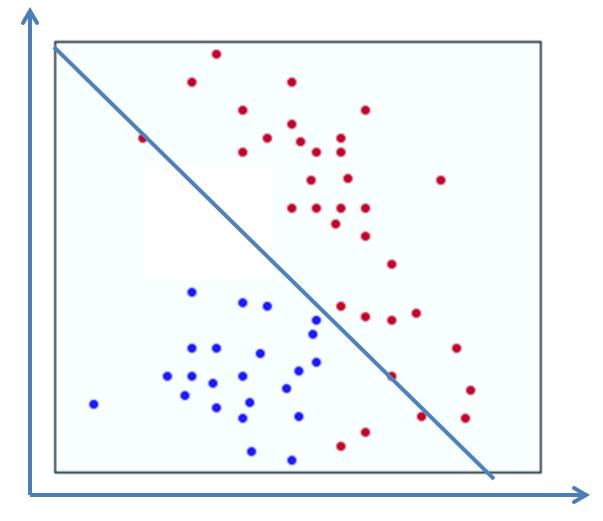
Topics Today

- Support Vector Machines (supervised classification)
- Random walker algorithm (manual-assisted segmentation)
- Graph cuts and Markov random fields (segmentation)
- Multi-atlas segmentation (registration-based segmentation)
- Deep neural networks (segmentation)

SUPPORT VECTOR MACHINES

Linear Classification



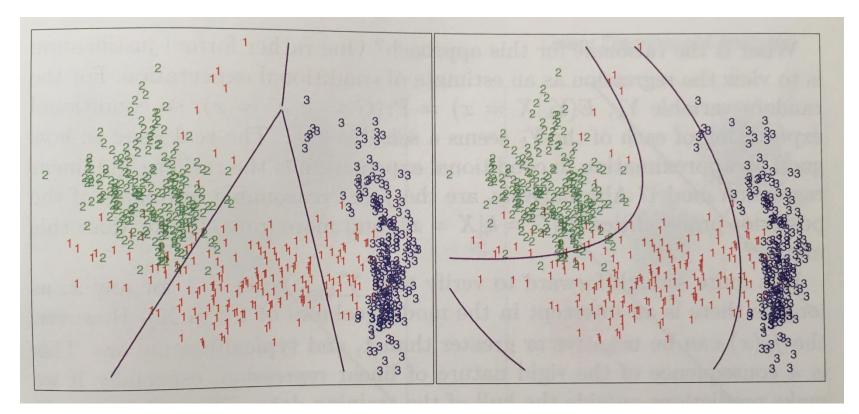


Linear classification means that Decision boundaries are linear

Image feature 1 (e.g., T1w value)

General Linear Boundaries

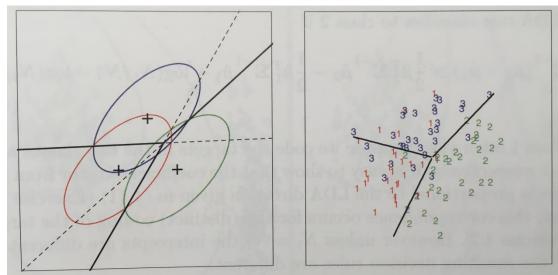
- Divide space into labeled regions
- Piecewise linear boundaries
- Linear in any monotone transformation
- Quadratic boundaries



Linear Discriminant Analysis (LDA)

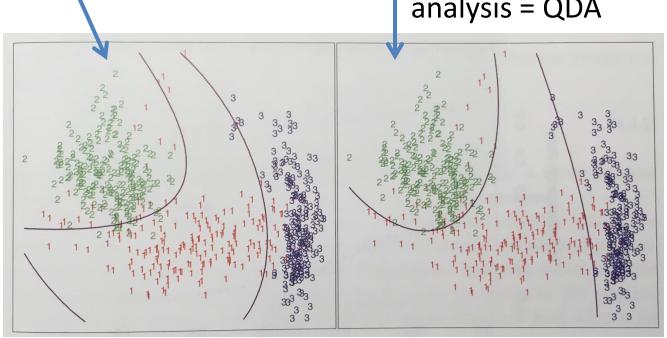
- Predictor G(x) takes on values 1, ... K
- Find discriminant function $\delta_k(x)$ and
- $G(x) = \underset{k}{\operatorname{argmax}} \delta_k(x)$

- Linear discriminant analysis
 - Each class is multivariate
 Gaussian with the same
 covariance matrix
 - Log ratio between probabilities yields linear boundaries



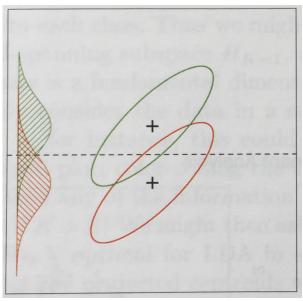
Quadratic Boundaries

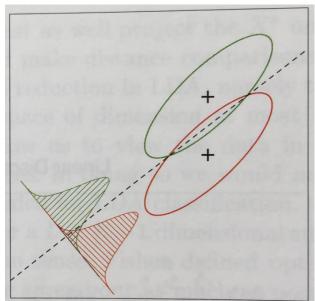
- Use LDA in 5-dimensional space: $x_1, x_2, x_1x_2, x_1^2, x_2^2$
 - Linear in 5-D, quadratic in original space
- Assume covariance matrices are different
 - Leads naturally to quadratic boundaries
 - Quadratic discriminantanalysis = QDA



Dimensionality Reduction

- With K centroids, the linear decision rule can be made in (K-1)-dimensional space
- A correct projection of the N-D data points into K-1 dimensions is needed
- Consideration of the prior probabilities can be made in the (K-1)-D space



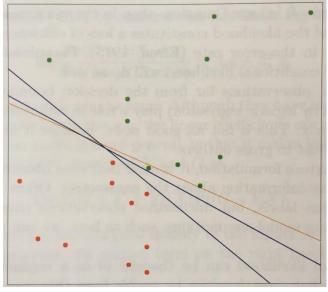


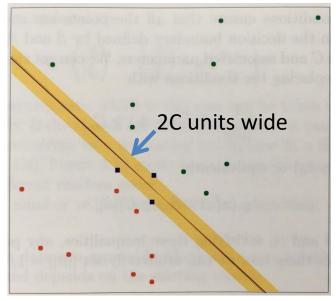
Credit: Hastie, 2001

Separating Hyperplanes

- Previous focus modeled all the points in each class
- Focus now on the points near the decision boundary
- Principle: A large margin on the training data will lead to good separation of the training data
- Maximize distance C from a line that separates the data
- Depends on fact that that such a line exists

Credit: Hastie, 2001





Support Vector Classifier

Permit some points support points—to be on the "wrong side" of the margin

Separable

- Tuning parameter (tolerance) γ chosen small yields a larger margin involving points far away
- Defined still as a linear classifier

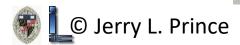
Non-separable

 ξ_5^* margin

 $x^T \beta + \beta_0 = 0$

 $x^T \beta + \beta_0 = 0$

Credit: Hastie, 2001



margin

Support Vector Machine

 Move from linear classifiers to higher-order using transformations via basis functions

$$h(x_i) = (h_1(x_i), h_2(x_i), ..., h_M(x_i))$$

 Replacing these in the support vector classifier yields functions that depend only on

$$K(x, x') = \langle h(x), h(x') \rangle$$

- Never need to compute $h(x_i)$ at all
 - So-called "kernel trick"

- Popular kernels:
 - d degree polynomial

$$K(x, x') = (1 + \langle x, x' \rangle)^d$$

Radial basis function

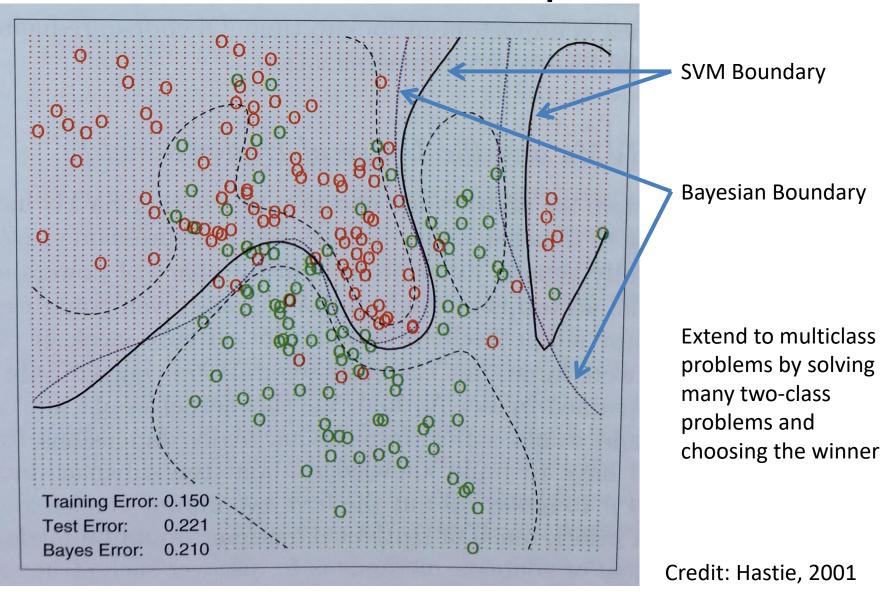
$$K(x, x') = \exp(-\frac{\|x - x'\|^2}{c})$$

Neural network

$$K(x, x') = \tanh(\kappa_1 \langle x, x' \rangle + \kappa_2)$$

- Large γ leads to squiggly boundary (and overfitting)
- Estimate γ by cross-validation

SVM Example



RANDOM WALKER ALGORITHM

Random Walks

Choose seed pixels with labels

Random Walks

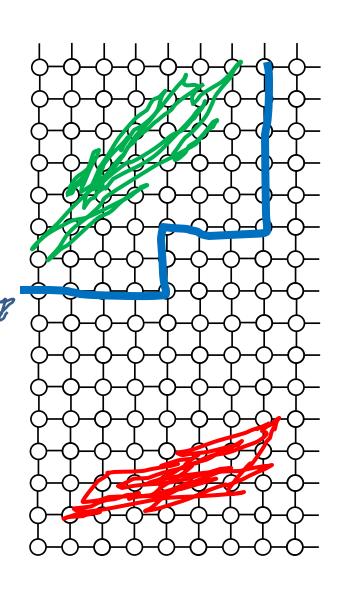
- Choose seed pixels with labels ℓ_1, \dots, ℓ_K
- Define edge probabilities as

$$w_{ij} = \exp\left(-\beta(f(\mathbf{p}_i) - f(\mathbf{p}_j)^2\right)$$

where f is image intensity

- Note: $0 \le w_{ij} \le 1$

 x_{ij} small on edge



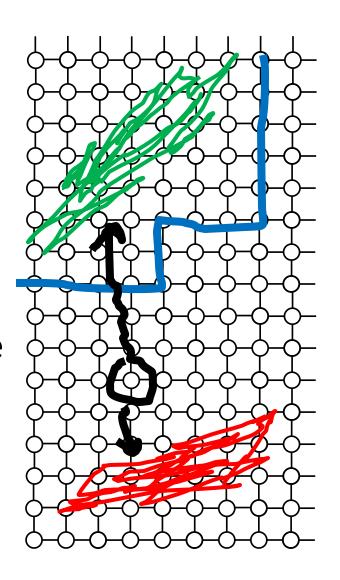
Random Walks

- Choose seed pixels with labels ℓ_1, \dots, ℓ_K
- Define edge probabilities as

$$w_{ij} = \exp\left(-\beta(f(\mathbf{p}_i) - f(\mathbf{p}_j)^2\right)$$

where f is image intensity

- Note: $0 \le w_{ij} \le 1$
- Compute for each nonseed pixel the probability that a random walk reaches seed ℓ_k first
- Segmentation is the label with the highest probability



The Dirichlet Problem

 Probabilities are found by finding x (all pixel probabilities) that minimizes

$$D(\mathbf{x}) = \frac{1}{2} \sum_{e_{ij} \in E} w_{ij} (x_i - x_j)^2 = \frac{1}{2} \mathbf{x} L \mathbf{x}$$

Where L is the combinatorial Laplacian matrix

$$L_{ij} = \begin{cases} d_i, & \text{if } i = j \\ -w_{ij}, & \text{if } v_i \text{ and } v_j \text{ are adjacent nodes} \\ 0, & \text{otherwise} \end{cases}$$

• Where d_i is sum of all edge weights incident on pixel i

Solving the Dirichlet Problem

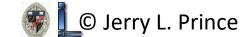
- Seed pixels are in V_M . Unmarked pixels are in V_U .
- Seeds may have different labels

• Then
$$D(\mathbf{x}_U) = \frac{1}{2} \begin{bmatrix} x_M^T & x_U^T \end{bmatrix} \begin{bmatrix} L_M & B \\ B^T & L_U \end{bmatrix} \begin{bmatrix} x_M \\ x_U \end{bmatrix}$$
$$= \frac{1}{2} (x_M^T L_M x_M + 2x_U^T B_T x_M + x_U^T L_U x_U)$$

• Differentiate with respect to x_U and set equal to zero, leading to

$$L_U x_U = -B^T x_M$$

 This amounts to <u>solving a modified Laplace's equation</u> with boundary conditions (the seed potentials)



Multiple Labels

- The label s of seed v_j is given by $Q(v_i)$
- Define

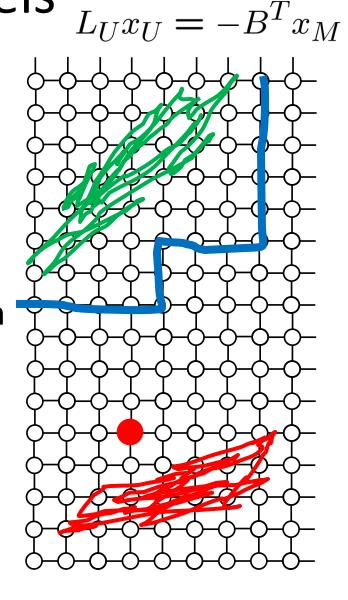
$$m_j^s = \begin{cases} 1 & \text{if } Q(v_j) = s, \\ 0 & \text{if } Q(v_j) \neq s. \end{cases}$$

 The probabilities for label s can then be found by solving

$$L_{U}x^{s} = -B^{T}m^{s}$$

- Repeat for all labels
- Assigned label at a given pixel is

$$\hat{l} = \arg \max_{s} x^{s}$$

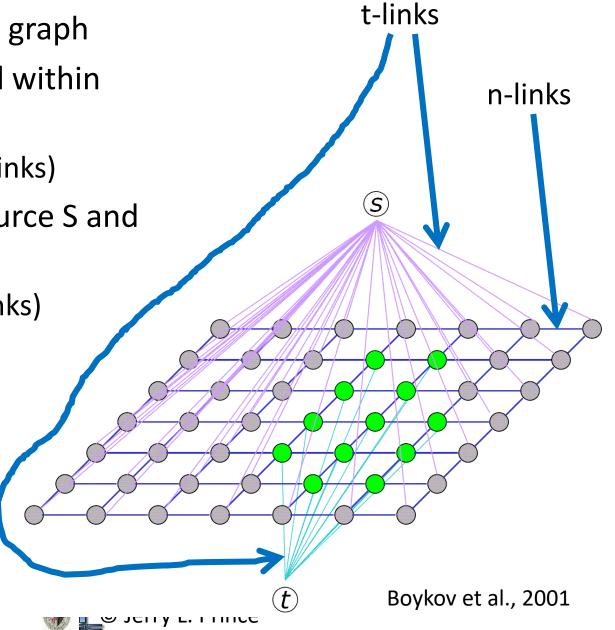




GRAPH CUTS SEGMENTATION

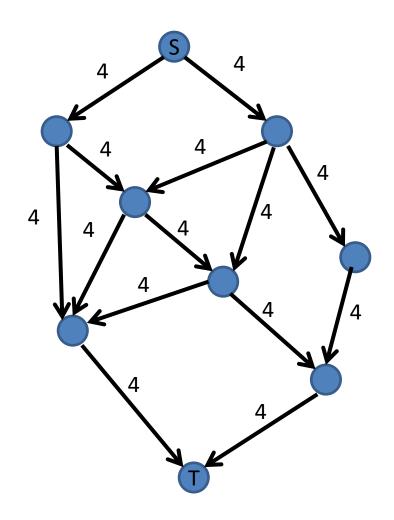
Graph Cuts Framework

- Pixels are nodes in a graph
- Pixels are connected within image
 - Neighbor links (n-links)
- Pixels connect to source S and sink T
 - Terminal links (t-links)
- Segmentation is produced by a graph cut
- Separates s and t



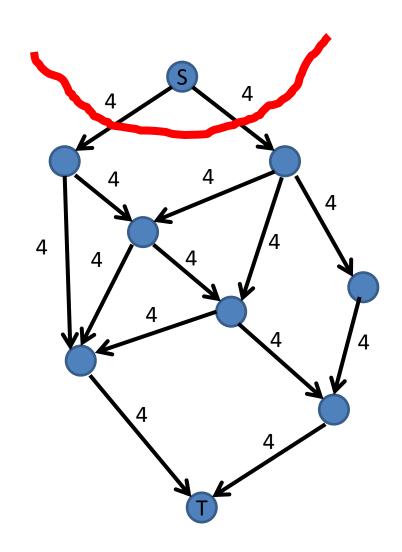
Principle of Max-Flow Min-Cut

- Consider a flow network from S to T with capacities on the directed edges
- What is the maximum flow out of S (and into T)?



Principle of Max-Flow Min-Cut

- Consider a flow network from S to T with capacities on the directed edges
- What is the maximum flow out of S (and into T)?
- It is equal to the sum of the edge weights (capacities) in the minimum cut
- (A "cut" separates the source from the sink)
- This problem can be solved exactly and rapidly using linear programming





Capacities on t-links

- Water flows from S to T
- Each pixel has:
 - Prob(foreground)
 - Prob(background)
- *S* t-links get capacities:

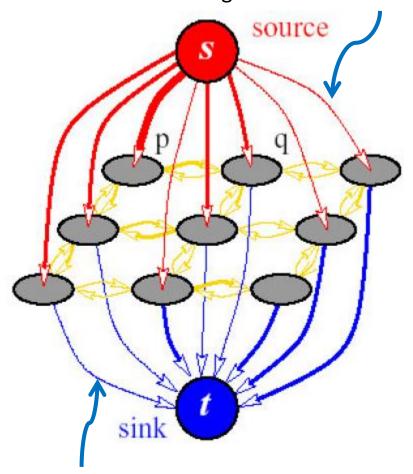
$$-R(p,S) = -\ln \text{Prob}(f)$$

• *T* t-links get capacities:

$$-R(p,T) = -\ln \text{Prob}(b)$$

- S to background flows easily
- Foreground to T flows easily

Water has difficulty flowing to the foreground

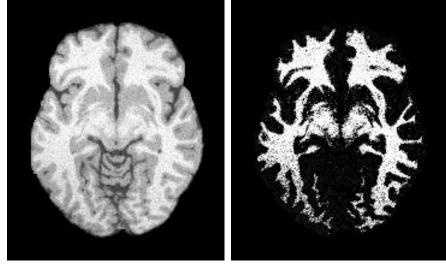


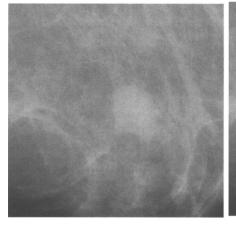
Water has difficulty flowing from the background

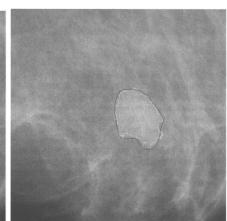


Foreground/Background Probabilities

- Could use memberships from fuzzy K-means posterior densities from EM method
- Could use fuzzy segmentation with manual assist







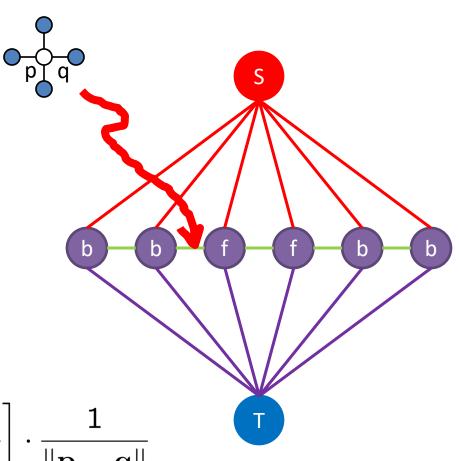
$$\begin{array}{c|c}
\Gamma(\mathsf{p}) \\
\hline
\end{array}$$

$$\Gamma(\mathbf{A} - \mathbf{B}) = \frac{1}{1 + \beta |\mathbf{A} - \mathbf{B}|}$$

Capacities on n-links?

- We want to cut at boundaries → capacity should be small on boundaries
- Let f(p) be a "feature" at pixel p (could be intensity)
- Suitable boundary capacities are

$$B_{p,q} = \exp\left[-\frac{\|f(\mathbf{p}) - f(\mathbf{q})\|^2}{2\sigma^2}\right] \cdot \frac{1}{\|\mathbf{p} - \mathbf{q}\|}$$



What does the min cut do?

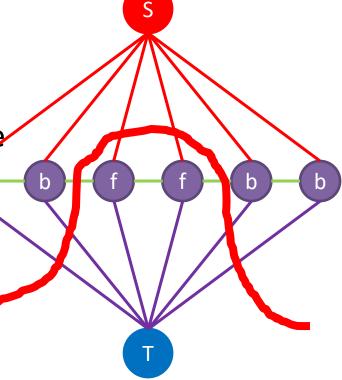
 Find cut C separating S and T with minimum edge cost

$$E(C) = \lambda \left(\sum_{p \in S_c} R(\mathbf{p}, S) + \sum_{p \in T_c} R(\mathbf{p}, T) \right) + \sum_{(p,q) \in N_c} B_{p,q}$$

• S_c are the edges in the S t-links that are cut by C

T_c are the edges in the T t-links that are cut by C

• N_c are the edges in the N n-links that are cut by C



👸 🔔© Jerry L. Prince

Solving the Max Flow Problem

- Classical Floyd-Fulkerson algorithm
 - Find the minimal cost path from S to T
 - Increase flow until edge with min weight saturates
 - Reduce remaining edges on path by W_{min}
 - Remove zero capacity edges and repeat
- Boykov and Kolmogorov's algorithm can be faster

Markov Random Fields

- Bayesian image restoration $\hat{f} = \arg \max_{f} P(f|g)$
- Posterior density is $P(\mathbf{f}|\mathbf{g}) \propto P(\mathbf{g}|\mathbf{f})P(\mathbf{f})$
- Image corrupted by Gaussian noise

$$P(\mathbf{g}|\mathbf{f}) = \frac{1}{Z_1} \exp\left[-\frac{1}{2} \left((\mathbf{g} - \mathbf{f})^T \mathbf{\Sigma}^{-1} (\mathbf{g} - \mathbf{f}) \right) \right]$$

Prior probability

$$P(\mathbf{f}) = \frac{1}{Z_2} \exp\left(-U(\mathbf{f})\right)$$

Gibbs Distributions

- A clique in a graph is a collection of nodes that is fully connected (every node is connected to every other node)
- Gibbs distribution has

$$U(\mathbf{f}) = \sum_{c \in \mathcal{C}} V_c(\mathbf{f})$$

Simple smoothness:

$$V_c(f(\mathbf{p}), f(\mathbf{q})) = ||f(\mathbf{p}) - f(\mathbf{q})||^2$$

$$P(\mathbf{f}) = \frac{1}{Z_2} \exp(-U(\mathbf{f}))$$



Nearest neighbor is most common 4 neighbors in 2D 6 neighbors in 3D



Form of Posterior Density

 Posterior also has the form of a MRF

- Conditional:

$$P(\mathbf{g}|\mathbf{f}) = \frac{1}{Z_1} \exp\left[-\frac{1}{2} \left((\mathbf{g} - \mathbf{f})^T \mathbf{\Sigma}^{-1} (\mathbf{g} - \mathbf{f}) \right) \right]$$

– Prior:

$$P(\mathbf{f}) = \frac{1}{Z_2} \exp \left(-\sum_{c \in \mathcal{C}} V_c(f(\mathbf{p}), f(\mathbf{q})) \right)$$

– Posterior:

$$P(\mathbf{f}|\mathbf{g}) \propto P(\mathbf{g}|\mathbf{f})P(\mathbf{f})$$
$$= \frac{1}{Z_3} \exp[-E(\mathbf{f})]$$

To maximize the posterior w.r.t.
 f is to minimize E(f)

Adapt for Segmentation

- f is a "label" or "cartoon" image
- g is a noisy observation of f

$$P(\mathbf{g}|\mathbf{f}) = \frac{1}{Z_1} \exp\left[-\frac{1}{2} \left((\mathbf{g} - \mathbf{f})^T \mathbf{\Sigma}^{-1} (\mathbf{g} - \mathbf{f}) \right) \right]$$
$$= \frac{1}{Z_1} \exp\left[-\frac{1}{2\sigma^2} \sum_{i=1}^{J} (g_i - f_i)^2 \right]$$

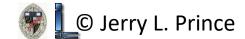
Posterior energy to minimize

$$E(\mathbf{f}) = \sum_{c \in \mathcal{C}} V_c(f(\mathbf{p}), f(\mathbf{q})) + \frac{1}{2\sigma^2} \sum_{i=1}^{J} (g_i - f_i)^2$$
$$= \sum_{c \in \mathcal{C}} V_c(f(\mathbf{p}), f(\mathbf{q})) + \lambda \sum_{i=1}^{J} D(f(\mathbf{p}))$$



Iterative Approach

- Specify an image labeling (foreground/background)
- Optimize a graph cut based on current labeling
- Repeat
- Two approaches for specifying the graph to cut
 - $-\alpha$ β swap
 - α expansion
- These methods use different graphs
- They both can be used for multiple labels (components in a scene, e.g., CSF, GM, WM)
- But lpha expansion has provable convergence properties



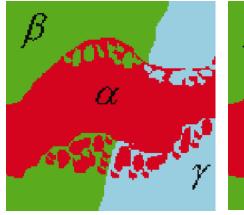
lpha - eta Swap

- Choose all pixels having either α or β label
 - E.g., could be foreground and background = all pixels
- Connect all neighbors with edges (n-links)

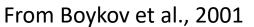
• All above nodes are connected to lpha (source) and eta (sink)

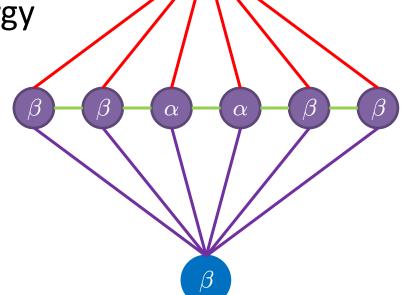
nodes

Find best label to reduce energy





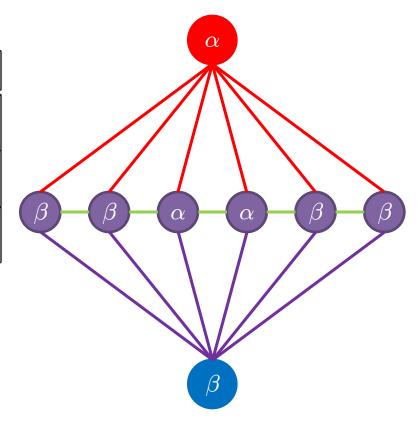




Weights for α - β Swap

Weights

edge	weight	for
t_p^{lpha}	$D_p(\alpha) + \sum_{\substack{q \in \mathcal{N}_p \\ q \notin \mathcal{P}_{\alpha\beta}}} V(\alpha, f_q)$	$p\in\mathcal{P}_{lphaeta}$
t_p^{eta}	$D_p(\beta) + \sum_{\substack{q \in \mathcal{N}_p \\ q \notin \mathcal{P}_{\alpha\beta}}} V(\beta, f_q)$	$p \in \mathcal{P}_{lphaeta}$
$e_{\{p,q\}}$	V(lpha,eta)	$\{p,q\}{\in}\mathcal{N} \ p,q{\in}\mathcal{P}_{lphaeta}$



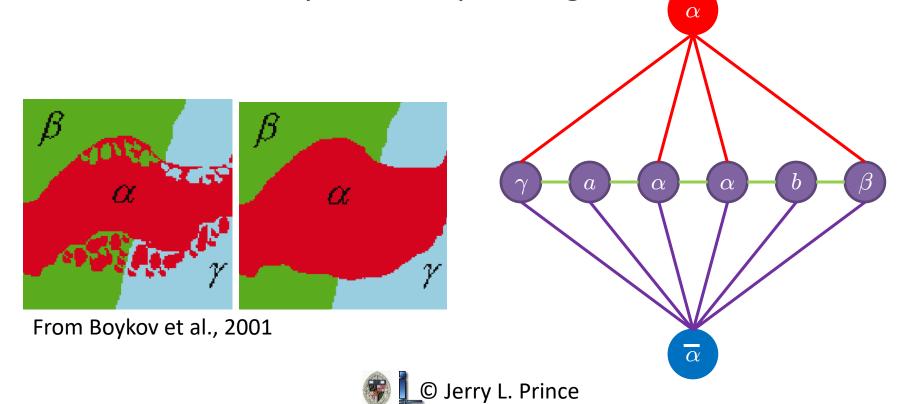
- Apply max flow / min cut to this
- This will relabel the graph/image with optimal descent
- Repeat the process with different labels until convergence



α Expansion

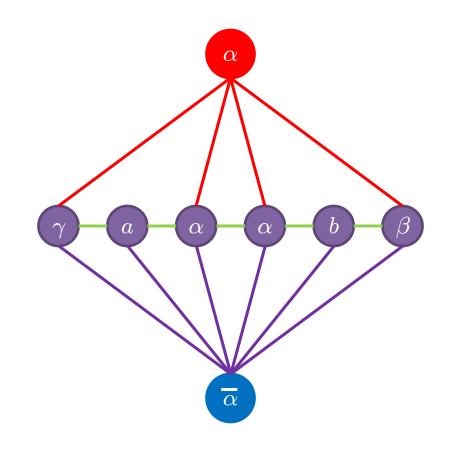
- Pick a single label lpha
- Find an expansion of α in all other labels that reduces the energy

Introduce auxiliary labels separating current partition



α Expansion Weights

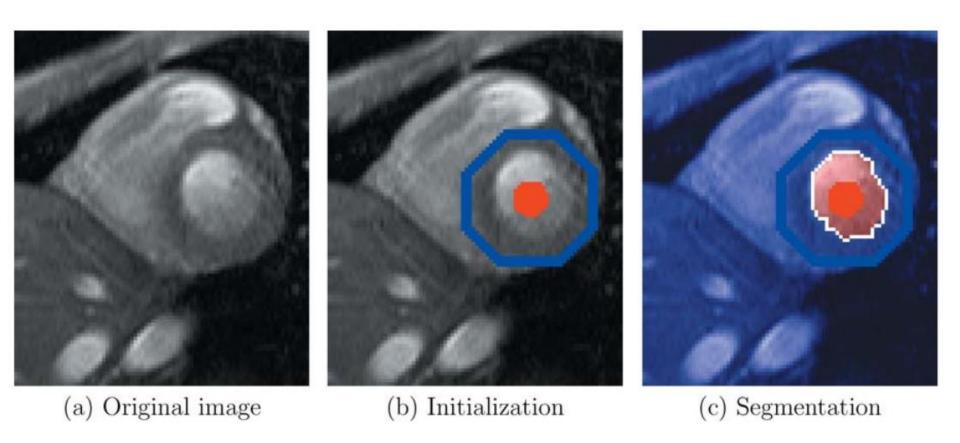
edge	weight	for
$t_p^{ar{lpha}}$	∞	$p \in \mathcal{P}_{lpha}$
$t_p^{ar{lpha}}$	$D_p(f_p)$	$p \not\in \mathcal{P}_{\alpha}$
t_p^{lpha}	$D_p(\alpha)$	$p \in \mathcal{P}$
$e_{\{p,a\}}$	$V(f_p, \alpha)$	
$e_{\{a,q\}}$	$V(\alpha, f_q)$	$\{p,q\} \in \mathcal{N}, \ f_p \neq f_q$
$t_a^{ar{lpha}}$	$V(f_p, f_q)$	
$e_{\{p,q\}}$	$V(f_p, \alpha)$	$\{p,q\}\in\mathcal{N},\;f_p=f_q$



From Boykov et al., 2001



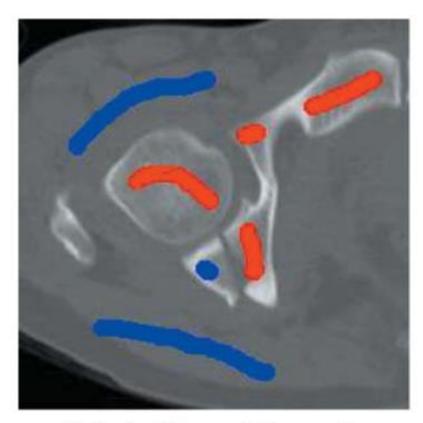
Example 1



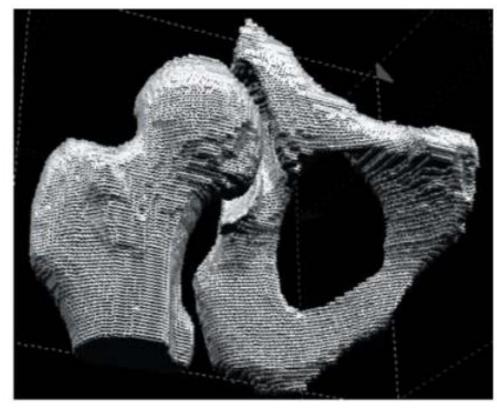
Credit: Boykov and Funka-Lea, 2006



Example 2



(a) A slice with seeds



(b) 3D object

Credit: Boykov and Funka-Lea, 2006

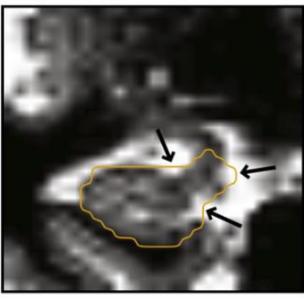


Example 3

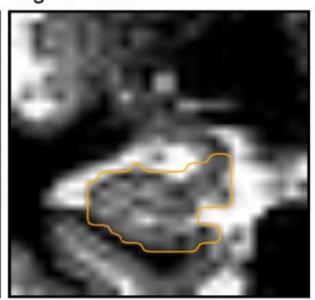
(a) Graph-cut-based hippocampus segmentation

Hippocampus segmentation

(b) Multi-atlas-based hippocampus segmentation



(c) Manual hippocampus segmentation



Credit: van der Lijn et al., 2008

MULTI-ATLAS SEGMENTATION

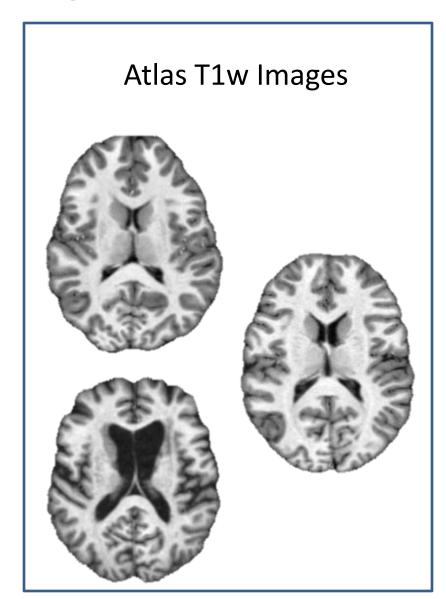
Credit: Blake Dewey



Multi-Atlas Segmentation

Subject T1w Image

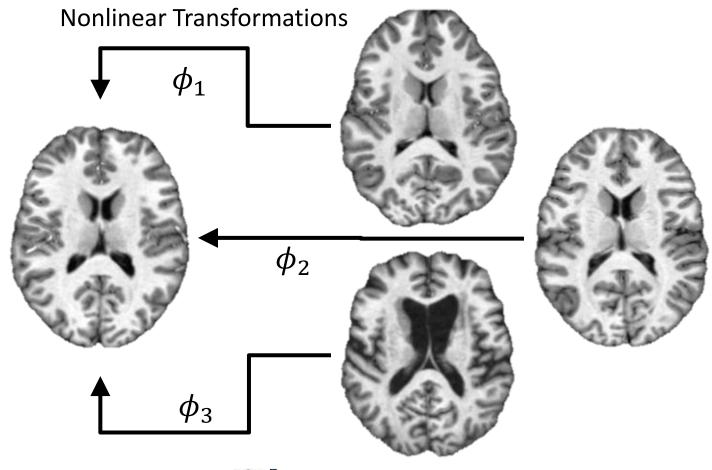




Learn Deformable Registrations

Subject T1w Image

Atlas T1w Images

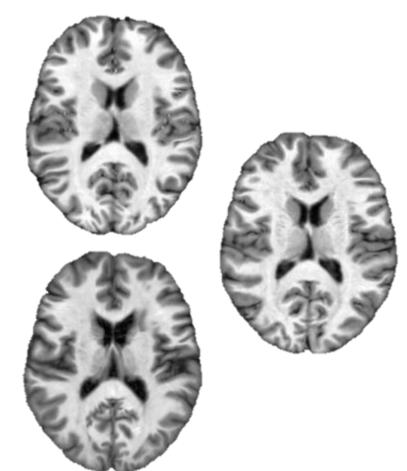


Apply Nonlinear Transformations

Subject T1w Image

These "look" like the subject—they are in registration with it...mostly



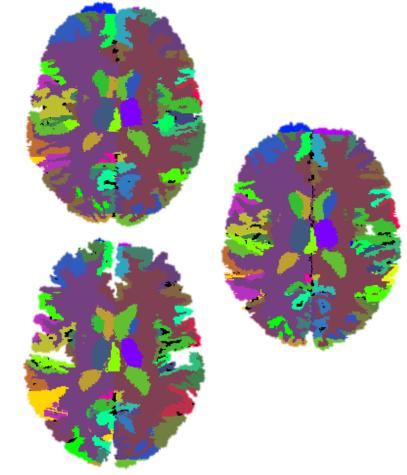


Apply Transformations to Labels

Subject T1w Image

The registered labels have the anatomy of the subject...mostly



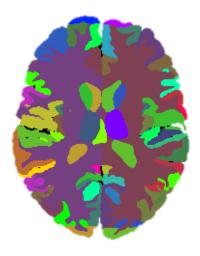


Fuse the Labels Into One Label Map

Subject T1w Image



Multi-Atlas Segmentation



Majority vote is fastest way to fuse labels, but probabilistic fusion is better

Comments on Multi-atlas Segmentation

- Registration is not perfect
 - Single registration is flawed
 - Multiple atlases are needed
 - Atlas selection could be added
 - Method is dependent on quality of registration
- Label fusion is key
 - Majority vote is fast
 - Statistical fusion methods are better, but slower

- Deformable registration is (typically) slow
 - 30 atlases is common
 - Parallelization is perfect so not 30x slower
- Topology not guaranteed
 - Anatomical realism not expected
 - Post-processing often used

DEEP NEURAL NETWORKS

Deep Learning

NEURAL NETWORK BASICS



Feed-Forward Neural Networks

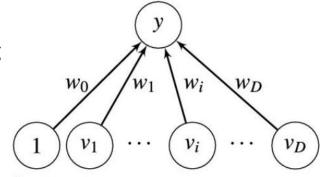
- Perceptron
 - Visible units (inputs v_i)
 - Trainable weights w_i
 - Bias w_0
 - Activation function $f(\cdot)$

- **Activation function**
 - Must be nonlinear
 - Logistic sigmoid for binary classification f(z) =

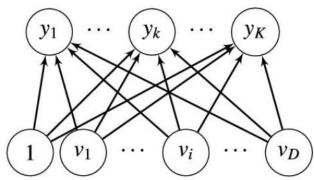
$$\frac{1}{1 + \exp[-z]}$$

$$y(\mathbf{v}; \Theta) = f\left(\sum_{i=1}^{D} v_i w_i + w_0\right) = f\left(\mathbf{w}^{\top} \mathbf{v} + w_0\right)$$

Credit: Deep Learning for Medical Image Analysis, Zhou, Greenspan, and Shen, 2017



A Single output (a.k.a. perceptron) An architecture of a single-layer neural network.

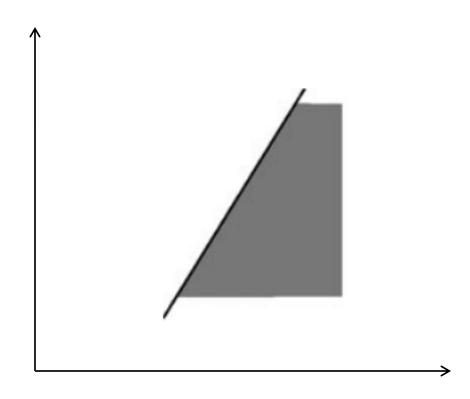


Multiple outputs



Linear Decision Boundary

$$decision = \begin{cases} 1 & y(v) > t \\ 0 & otherwise \end{cases}$$



Multi-Layer Neural Network

- Single layer is fundamentally limited by its linear separation function in a classification task
- Solution: Add more layers

$$y_k (\mathbf{v}; \Theta) = f^{(2)} \left(\sum_{j=1}^{M} W_{kj}^{(2)} f^{(1)} \left(\sum_{i=1}^{D} W_{ji}^{(1)} v_i \right) \right)$$

$$\mathbf{v} \qquad \mathbf{v}^{(1)} \rightarrow f^{(1)} \left(\mathbf{z}^{(1)} \right) = \mathbf{a} \qquad \mathbf{W}^{(2)} \rightarrow f^{(2)} \left(\mathbf{z}^{(2)} \right) = \mathbf{y}$$

Can add even more layers

$$y_k = f^{(L)} \left(\sum_{l} W_{kl}^{(L)} f^{(L-1)} \left(\sum_{m} W_{lm} f^{(L-2)} \left(\cdots f^{(1)} \left(\sum_{i} W_{ji}^{(1)} x_i \right) \right) \right) \right)$$

Decision Boundaries in Multiple Layers

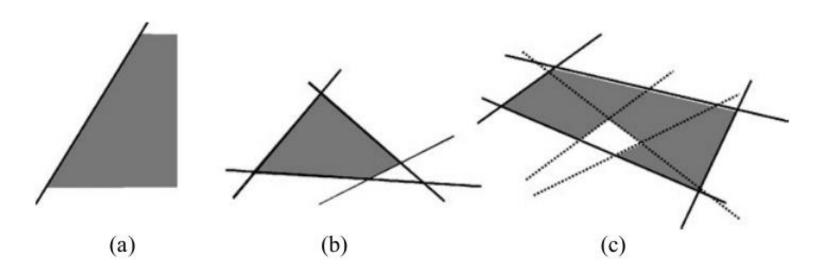
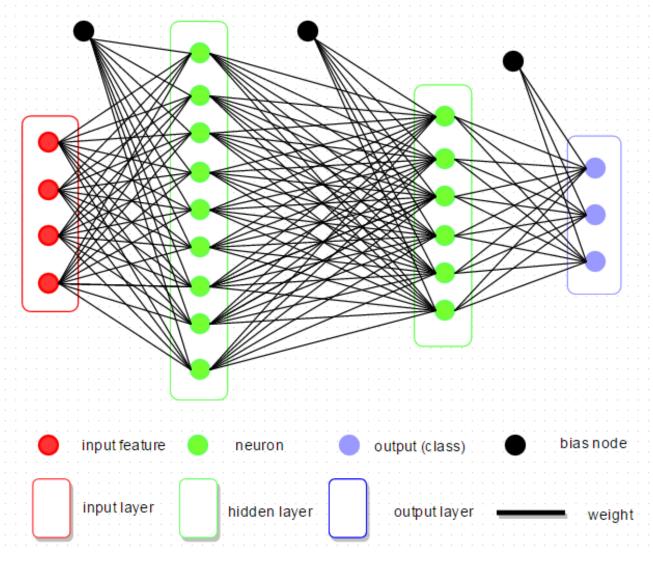
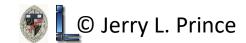


Fig. 12.18 (a) A single layer enables linear separation in feature space. (b) Adding nodes in an additional (hidden) layer, arbitrary convex decision boundaries can be represented. (c) With two hidden layers, convex figures can be combined to represent arbitrary concave decision boundaries

A 3-layers fully connected neural network (DNN)



https://www.r-bloggers.com/r-for-deep-learning-i-build-fully-connected-neural-network-from-scratch/



Activation Functions f(z)

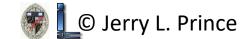
- Must be nonlinear
 - Otherwise the entire network is just a linear weight matrix
 - Ideally "squashes" real line into a small range of numbers
 - Should be differentiable (but this is violated all the time!)
- Logistic sigmoid

$$\sigma(z) = \frac{1}{1 + \exp[-z]}$$

- Range is [0,1]
- Hyperbolic tangent

$$\tanh(z) = \frac{\exp[z] - \exp[-z]}{\exp[z] + \exp[-z]}$$

- Range is [-1,1]



Learning in Feed-Forward NNs

- Fundamental principle is error minimization
- Training set

$$-\{x_n, t_n\}, n = 1, ..., N$$

- Observation $x \in \mathbb{R}^D$
- Class indicator vector $t \in \{0,1\}^K$
 - This identifies which neuron *should* fire for a given training example

 For K-class classification use cross-entropy error function

$$E(\Theta) = -\frac{1}{2} \sum_{n=1}^{N} \sum_{k=1}^{K} t_{nk} \ln y_{nk}$$

- t_{nk} is the k-th element of the n-th indicator vector
- y_{nk} is the k-th element of the NN prediction vector for $oldsymbol{x}_n$

Gradient of Error Function

Use the chain rule as follows

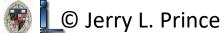
$$\frac{\partial E}{\partial \mathbf{W}^{(l)}} = \frac{\partial E}{\partial \mathbf{a}^{(L)}} \frac{\partial \mathbf{a}^{(L)}}{\partial \mathbf{a}^{(L-1)}} \cdots \frac{\partial \mathbf{a}^{(l+2)}}{\partial \mathbf{a}^{(l+1)}} \frac{\partial \mathbf{a}^{(l+1)}}{\partial \mathbf{a}^{(l)}} \frac{\partial \mathbf{a}^{(l)}}{\partial \mathbf{z}^{(l)}} \frac{\partial \mathbf{z}^{(l)}}{\partial \mathbf{W}^{(l)}}$$

• Where ∂

$$\frac{\partial \mathbf{a}^{(l+1)}}{\partial \mathbf{a}^{(l)}} = \frac{\partial \mathbf{a}^{(l+1)}}{\partial \mathbf{z}^{(l+1)}} \frac{\partial \mathbf{z}^{(l+1)}}{\partial \mathbf{a}^{(l)}} = f'\left(\mathbf{z}^{(l)}\right) \left(\mathbf{W}^{(l+1)}\right)^{\mathsf{T}}$$

FIGURE 1.3 Graphical representation of a backpropagation algorithm in an L-layer network.

• Gradient is $\nabla E(W) = \left[\frac{\partial E}{\partial W^{(1)}} ... \frac{\partial E}{\partial W^{(l)}} ... \frac{\partial E}{\partial W^{(l)}} \right]$

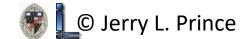


Gradient Descent = Backpropagation

Update coefficients using

$$\mathbf{W}^{(\tau+1)} = \mathbf{W}^{(\tau)} - \eta \nabla E \left(\mathbf{W}^{(\tau)} \right)$$

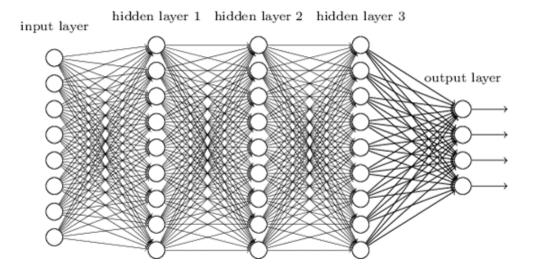
- η is called the "learning rate"
- Batch gradient descent
 - Evaluate and update using all training samples
- Stochastic gradient descent
 - Evaluate and update on individual training samples selected randomly
- Mini-batch gradient descent
 - Evaluate and update on small sets of samples



Problems with Deep Neural Networks

Problems:

- can have millions of parameters (weights)
- Ignores structure of images
- Training is slow



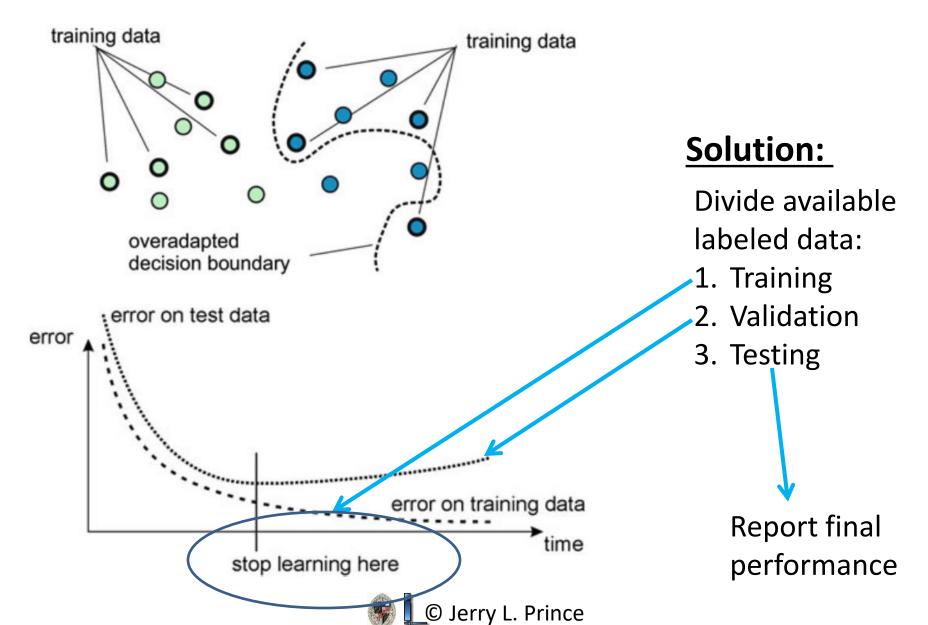
Solutions

- Use local connectivity
- Share weights via translations
- Use rectified linear unit (ReLU) as nonlinearity
- Use a simple optimizer
- Use unsupervised pretraining
- Use larger data sets
- Use GPUs

http://www.rsipvision.com/exploring-deep-learning/



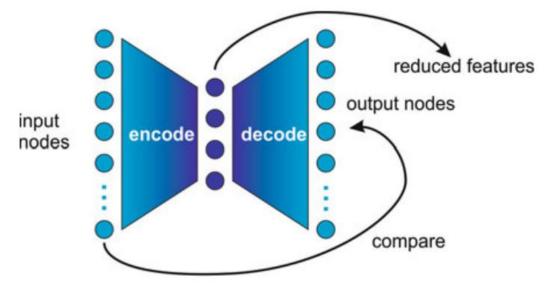
Large Problem: Overfitting

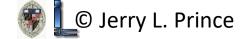


Principle of Autoencoders

- How to use MLPs as "feature generators"
- Reduce number of nodes and try to reconstruct *itself*
- Unsupervised NNs

- No training outputs (classes) are needed
- Gets at the question: what are the features key to describe these images/data?





Deep Learning

CONVOLUTIONAL NEURAL NETWORKS

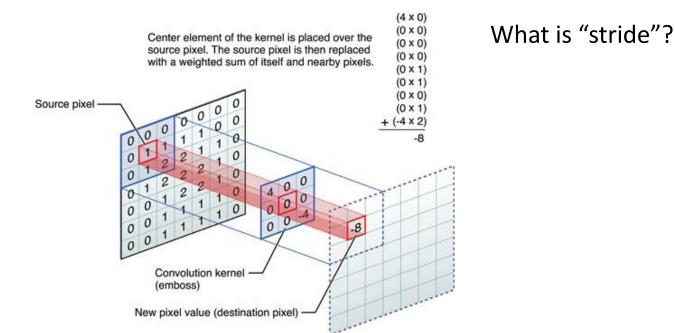


Convolutional Neural Networks (Key #1)

- Key idea #1: "convolution" (relates to data locality)
 - Localized connectivity

Use the same coefficients, but shifted, within the same

layer



https://developer.apple.com/library/content/documentation/Performance/Conceptual/vImage/ConvolutionOperations/ConvolutionOperations.html



Convolutional Neural Networks (Key #2)

- Key idea #2: "max pooling"
 - Reduces dimension
 - Keeps largest "responses"
 - Reduces shift dependence

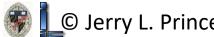
Single depth slice

x T	1	1	2	4
	5	6	7	8
	3	2	1	0
	1	2	3	4

max pool with	2x2 filters
and stride 2	

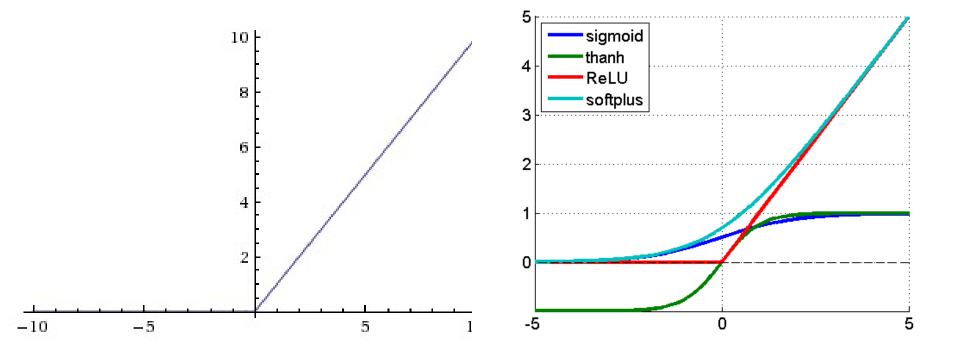
6	8
3	4

http://cs231n.github.io/convolutional-networks/



Convolutional Neural Networks (Key #3)

- Key idea #2: "ReLU activation function"
 - Trains orders of magnitudes faster

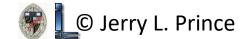


http://cs231n.github.io/neural-networks-1/



Optimization in ConvNets

- Choose a loss (error, cost) function
- Gradient descent = standard backpropagation
 - Computes gradient against all the training data
- Mini-batch gradient descent
 - Choose 100 or 256 examples from the training data (of 1.2 million)
 - Compute gradient against mini-batch
- Stochastic gradient descent
 - Compute gradient against only one training example
 - Not common because it is not as efficient
- Dropout
 - Randomly drop neurons with probability p during training
 - At test time use all neurons and multiply each activation by p to account for the scaling
- Batch normalization (and instance normalization)
 - Solves "internal covariate shift" problem; accelerates training



AlexNet (2012, started modern era)

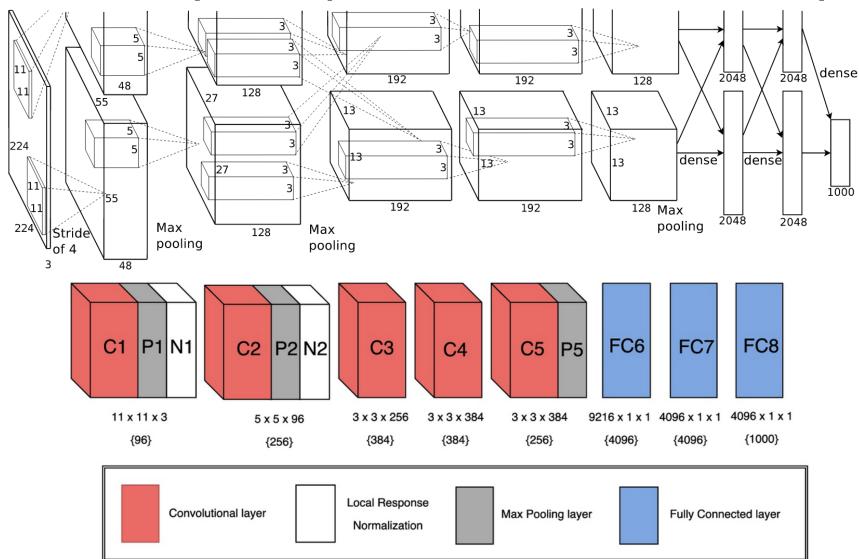
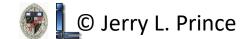


FIGURE 2.1 An illustration of the weights in the AlexNet model. Note that after every layer, there is an implicit ReLU nonlinearity. The number inside curly braces represents the number of filters with dimensions mentioned above it.



Using Pre-Trained CNNs

- AlexNet was successful in part because it was easy to retrain
- Fine-tuning
 - Download pre-trained AlexNet
 - Fix weights in early layers if task is similar
 - Re-train using SGD for new categories
- CNN activations as features
 - Use FC7 activation of an image as a generic feature descriptor
 - Better than SIFT or HoG features (so-called "hand-crafted" features)



Improving AlexNet

- AlexNet won ILSVRC challenge in 2012
- Overfeat won ILSVRC-2013
- GoogleNet won ILSVRC-2014
 - Added 1x1 convolutional layer after a regular convolutional layer
 - 1x1 is useful because it combines R,G,B color channels
- VGG-19 is a deep CNN
 - Stacks of smaller sized filters
- Deep Residual Networks (residual "blocks" are important now)
 - 152-200 layers
 - Instead of learning mapping h(x), learn f(x)-x, then later add f(x)+x
- Fully Convolutional Networks

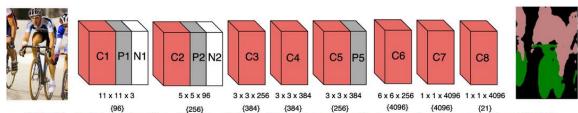


FIGURE 2.3 Fully Convolutional Net – AlexNet modified to be fully convolutional for performing semantic object segmentation on PASCAL VOC 2012 dataset with 21 classes.



SegNet: Encoder-Decoder Architecture

Features:

- 13 convolutional layers = first 13 in VGG16
- Discard fully connected layers; using only convolutional layers

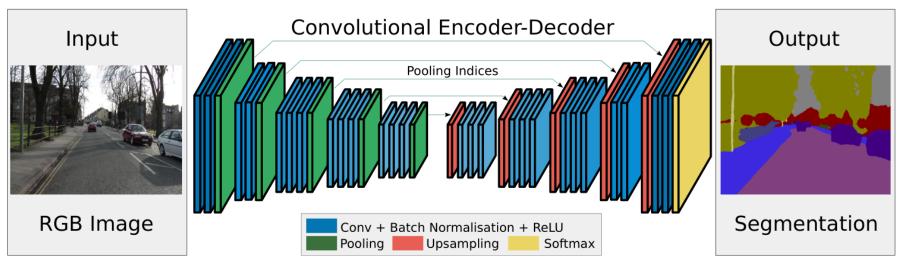


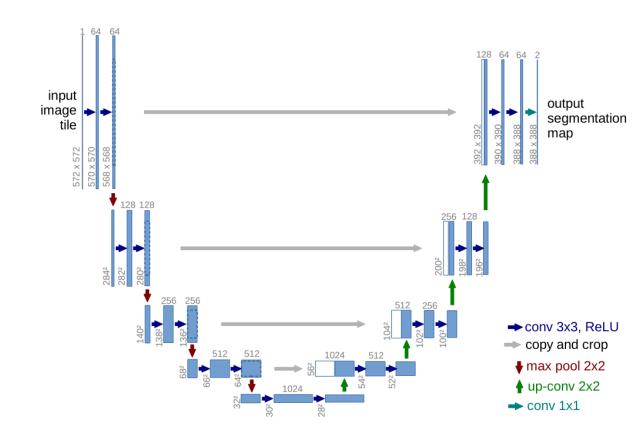
Fig. 2. An illustration of the SegNet architecture. There are no fully connected layers and hence it is only convolutional. A decoder upsamples its input using the transferred pool indices from its encoder to produce a sparse feature map(s). It then performs convolution with a trainable filter bank to densify the feature map. The final decoder output feature maps are fed to a soft-max classifier for pixel-wise classification.

Badrinarayanan, Vijay, Alex Kendall, and Roberto Cipolla. "Segnet: A deep convolutional encoder-decoder architecture for image segmentation." *arXiv preprint, 2015*

🏶 🛴 🛭 Jerry L. Prince

U-Net: CNNs for Biomedical Segmentation

- Features
 - Skip connections
 - Transfers
 entire
 feature map
 from
 encoder to
 decoder



Ronneberger, Olaf, Philipp Fischer, and Thomas Brox. "U-net: Convolutional networks for biomedical image segmentation." *International Conference on Medical Image Computing and Computer-Assisted Intervention*. Springer International Publishing, 2015.



Deep Learning

EXAMPLE: BRAIN MRI SEGMENTATION



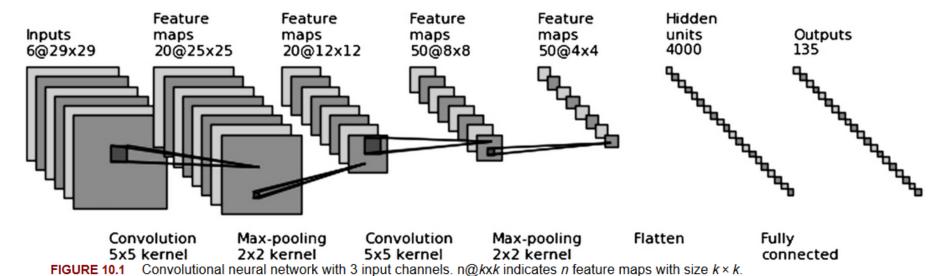
Case Example: Brain MRI Segmentation

- Chapter 10 in Deep Learning for Medical Image Analysis
 - Authors: Akshay Pai, Yuan-Ching Teng, Joseph Blair, Michiel Kallenberg, Erik B. Dam, Stefan Sommer, Christian Igel, and Mads Nielsen
- Application of CNN to Brain MRI Segmentation
- Major hurdles to overcome
 - 3D data are too large for CNNs of appreciable depth
 - Large variability in data
 - Too few training samples



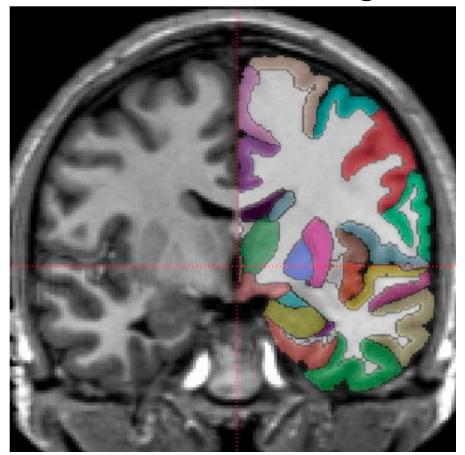
CNN Architecture

- Use tri-planar input images (two scales)
- All feature maps and convolutions are 2D
- ReLU is used for activation
- 135 classes are to be segmented



Datasets

- Input images are T1-weighted MRI
- Labels from the MICCAI 2012 multi-atlas challenge
 - 40 cortical labels
 - 94 non-cortical labels





CNN used in Experiment

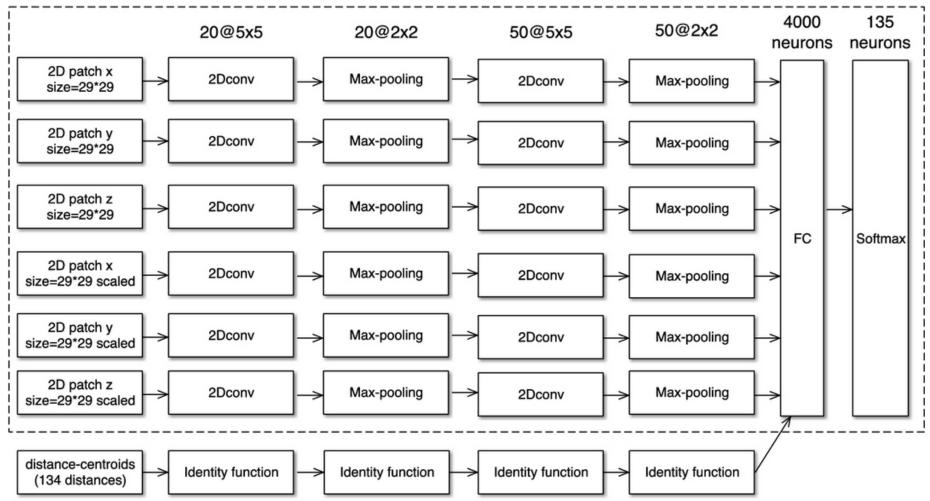
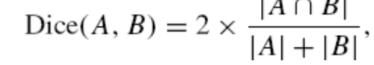


FIGURE 10.2 The convolutional neural network used in the experiment. The dotted box represents the architecture of CNN without centroids and the solid box (outermost) represents the architecture of the CNN with centroids as an input feature. There are 135 neurons in the softmax layer (instead of 134) since the background class is also included.



Training

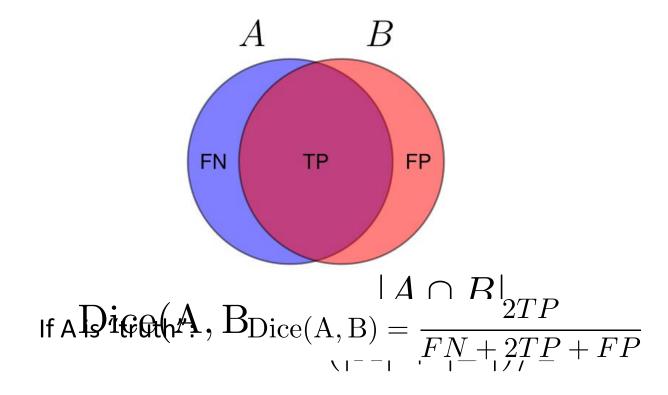
- Trained using 10 images
- Used remaining 5 for validation
- Split training into 4 parts (mini-batches) to fit in GPU
- Trained for 60 epochs (one epoch trains on n mini-batches)
- Randomly sampled 4000,000 voxels from training set and 200,000 voxels from validation for each epoch.
 - Validation set was used to detect overfitting; none was found
- Data from training and validation set combined and the network trained from 15 images for 10 epochs
- After training, classify images in test set
- Evaluate using Dice coefficient $Dice(A, B) = 2 \times$





Dice Overlap Measure

In imaging, each pixel/voxel has a potential object that we are trying to detect



Results

Compare to multi-atlas method with majority vote (Reg)

Table 10.3

The mean Dice score of the test set using different methods. Registration is the multi-atlas registration method; CNN without centroids is the CNN with 2 sets of tri-planar patches; CNN with centroids is the CNN with 2 sets of tri-planar patches and the distances of centroids

Method	Mean Dice score	Г	T	T	ı
Registration	0.724				
CNN without centroids	0.720	0.7			
CNN with centroids	0.736			+	
	Dice	0.6		+	-
		0.4	+		-
		0.3	+		

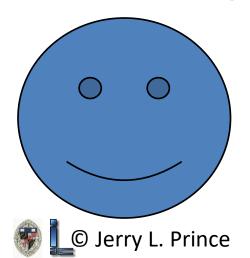
FIGURE 10.4 The Dice score of different methods. This box plot illustrates the variance in the Dice measure for each method.

cnn without centroid cnn with centroid

True Reg CNN With centroids**L**© Jerry L. Prince

Conclusion of Example

- Inferior to other methods in MICCAI 2012
- Could improve
 - Use convolution kernels at different scales
 - Use more training data
 - Reduce number of classes
 - Combine registration and CNN results
 - Choose a different architecture—e.g., deeper network



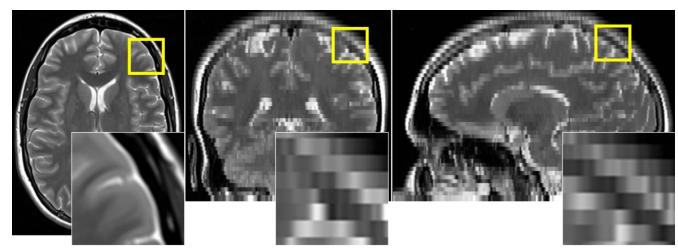
EXAMPLE: SUPER-RESOLUTION

Super-resolution in MRI

- Super-resolution: improve resolution by multiple observations of the same object
 - Multi-resolution
 - Multi-spectral
 - Multi-orientation

- Very long history in MRI
 - (Park et al, 2003)
 - (Greenspan, 2009)
 - (Van Reeth et al., 2012)
- Multi-orientation SR is most successful to date

Example: Good in-plane resolution, poor through-plane resolution

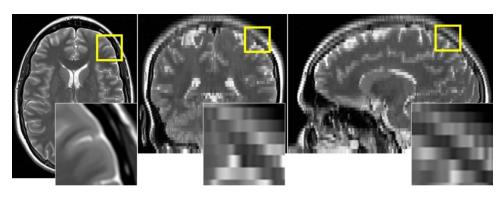


Single Image Super-resolution

- Single-image is highly desirable
 - Saves imaging time
 - Reduces impact of patient motion
- Additional desirable traits of super-resolution:
 - Do not require an atlas
 - No PSF inversion—i.e., no deconvolution

- Our approach:
 - Use self-training
 - Use Fourier burst accumulation (FBA)
 - Jog et al., MICCAI 2016
 - Zhao et al., ISBI 2018,
 MICCAI 2018

FBA: Delbracio and Sapiro, TCI, 2015

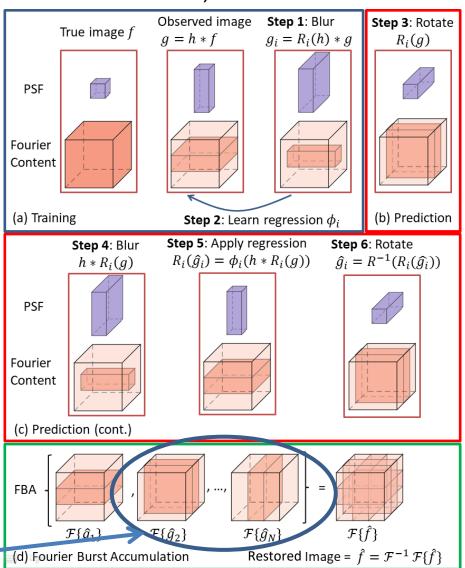


Self Super-Resolution (EDSSR) Jog et al. MICCAI 2016, Zhao et al. ISBI 2018, Zhao et al. MICCAI 2018

- Rotate observed image and apply 1-D blur
- Train EDSR (CNN) regression on 32x32 patches to restore original image patches
- Rotate image and apply regression multiple times
- **Apply Fourier burst** accumulation

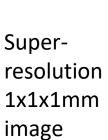
EDSR: B. Lim et al., CVPR, 2017. FBA: Delbracio et al. CVPR, 2015.

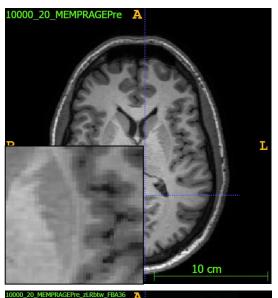
Synthetic images (using EDSR)

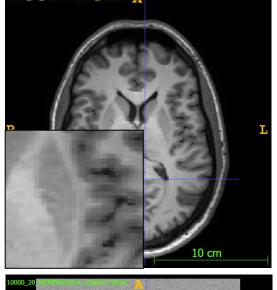


EDSSR Result: Axial View

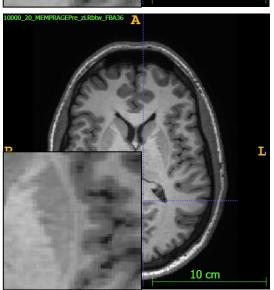
Original 1x1x1mm image

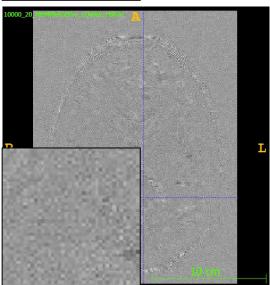






Blurred 1x1x3mm image

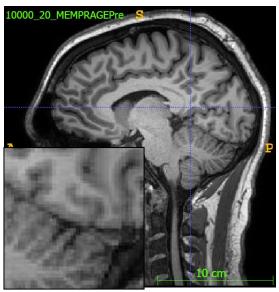




Difference image

EDSSR Result: Sagittal View

Original 1x1x1mm image

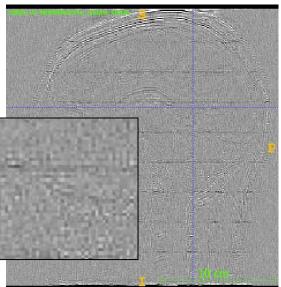




Blurred 1x1x3mm image

Superresolution 1x1x1mmimage

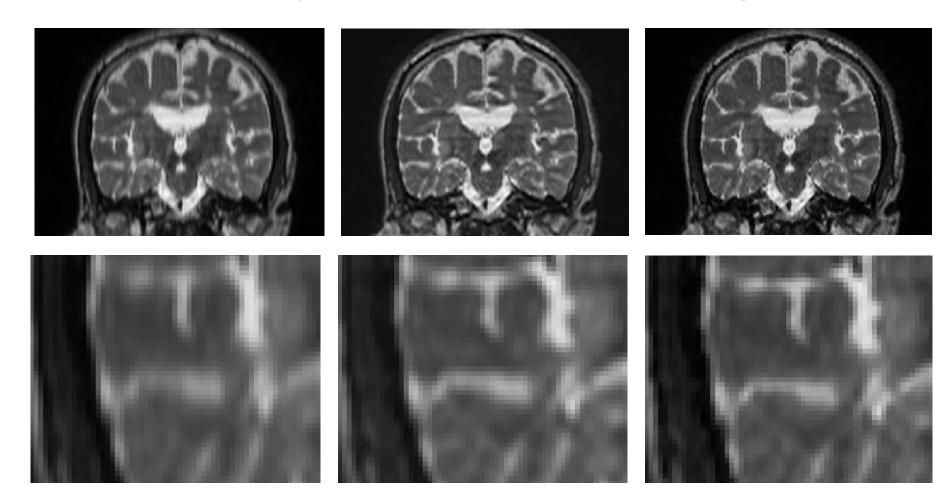




Difference image



Example on Real LR Image



B-Spline
Original: 0.83x0.83x2.20 mm

SSR (Jog et al.)

Super-res: 0.83x0.83x0.83 mm

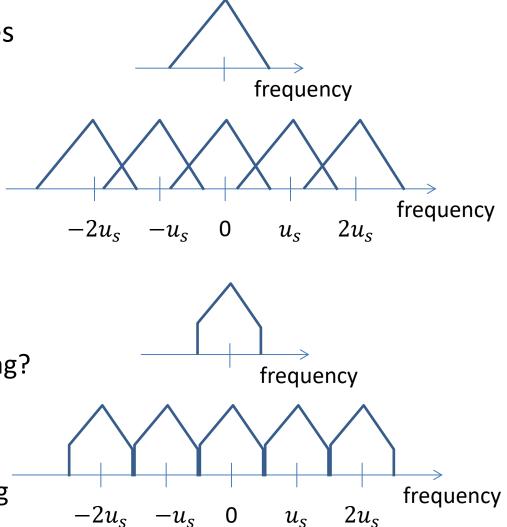
EDSSR (Zhao et al.)



Credit: Zhao et al., ISBI 2018 90

Aliasing and Anti-aliasing

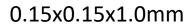
- Spatial undersampling causes aliasing
- Blurring signal before sampling is anti-aliasing
- Consider 2D MRI
 - Contiguous slices with slice thickness = slice separation
 - Approx 3/4 of all MRI
 - Slice thickness = anti-aliasing?
- Slice profile is not effective anti-aliasing
 - 2D MRI suffers from aliasing

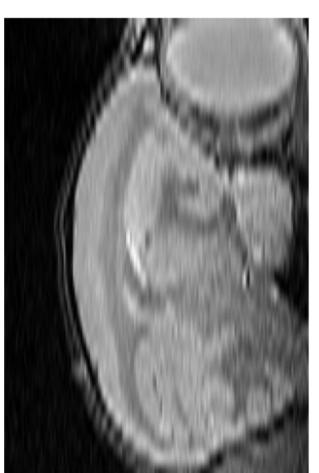


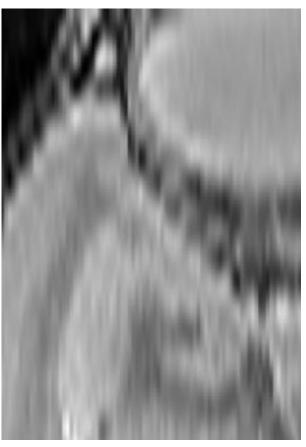
 u_{s}

Evidence of Aliasing





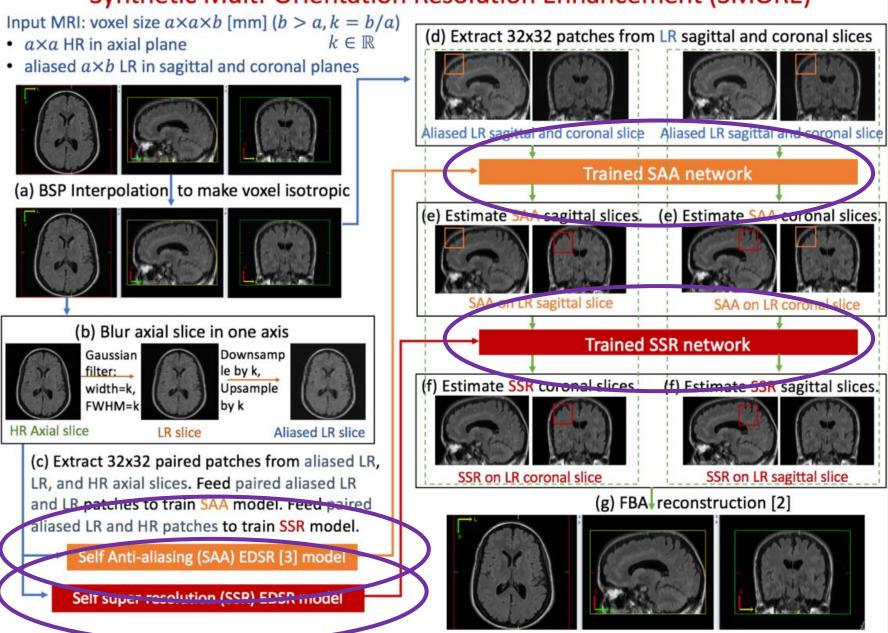




Mamoset brain data courtesy of Dzung Pham, HJF



Synthetic Multi-Orientation Resolution Enhancement (SMORE)



Marmoset Brain

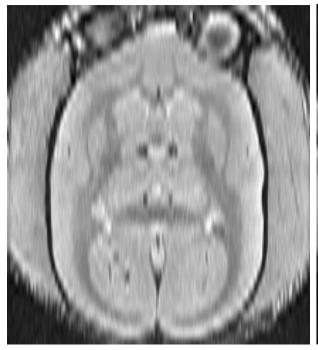
- 0.15x0.15x1.0mm
- Proton density weighted

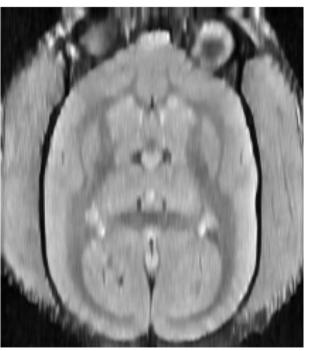
- k = 6.6667
- Aliasing is prominent

B-spline Interpolation

EDSSR Super-resolution

SMORE Super-resolution





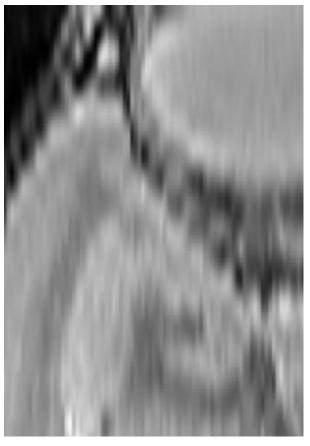


Marmoset Close Up

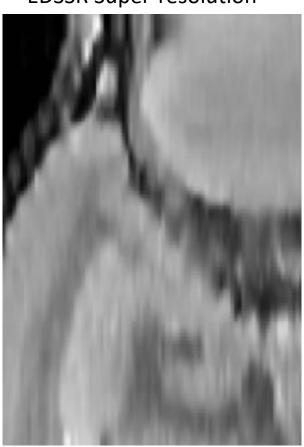
B-spline Interpolation EDSSR Super-resolution SMORE Super-resolution

Marmoset Zoomed Even More

B-spline Interpolation



EDSSR Super-resolution



SMORE Super-resolution



Comments on EDSSR and SMORE

Advantages:

- No external atlas required
- No contrast matching is necessary
- Single stack of images is the only requirement
- Save imaging time; avoid complications from motion

Disadvantages:

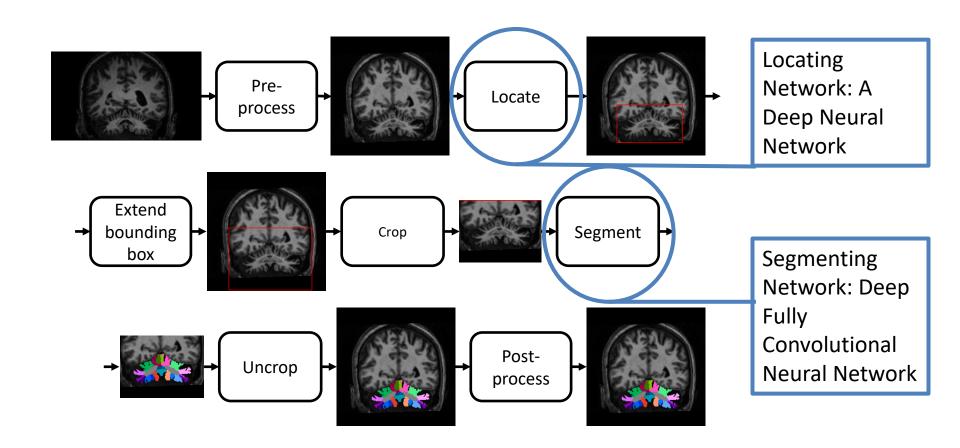
- Requires on-line training → time consuming
 - Can be made faster with pre-training, transfer learning
- Achieves in-plane resolution, no higher
- Requires intensity inhomogeneity correction (N4)

EXAMPLE: CEREBELLUM PARCELLATION

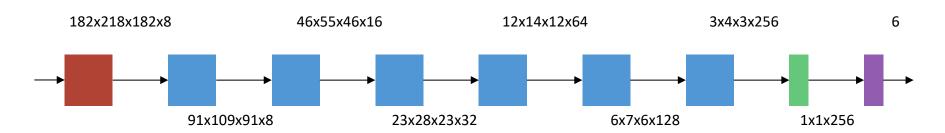
NEW METHOD USING DEEP NETWORKS

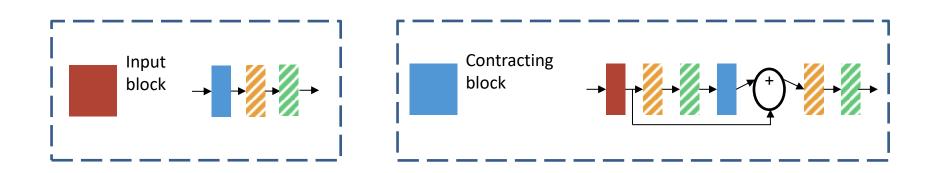


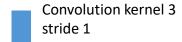
Block Diagram

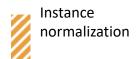


Locating Network

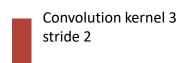


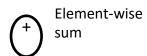


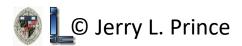




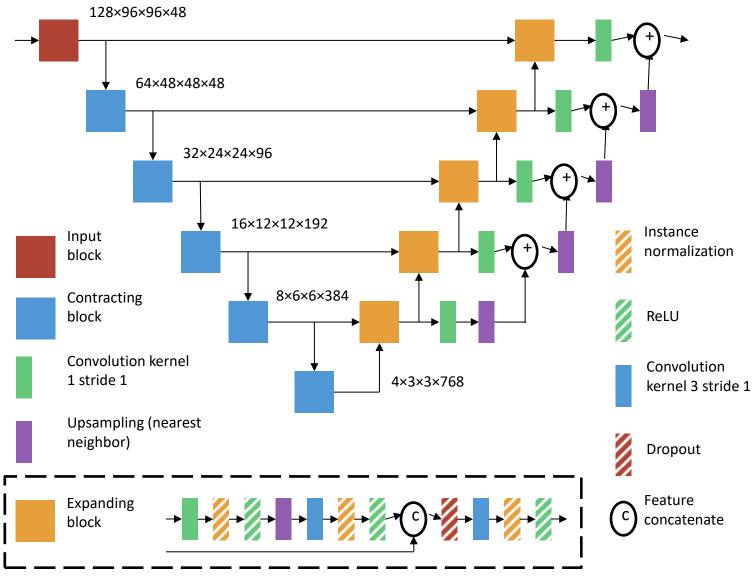




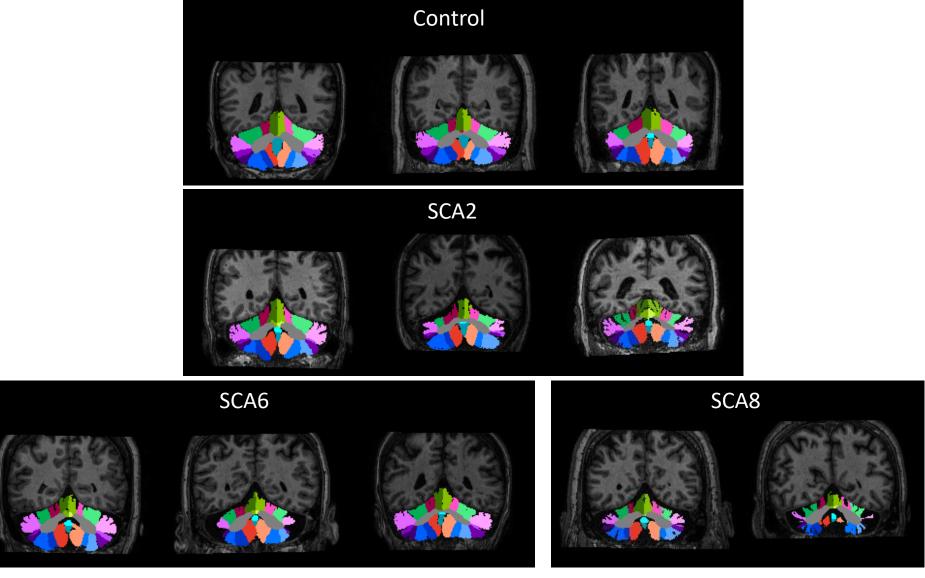




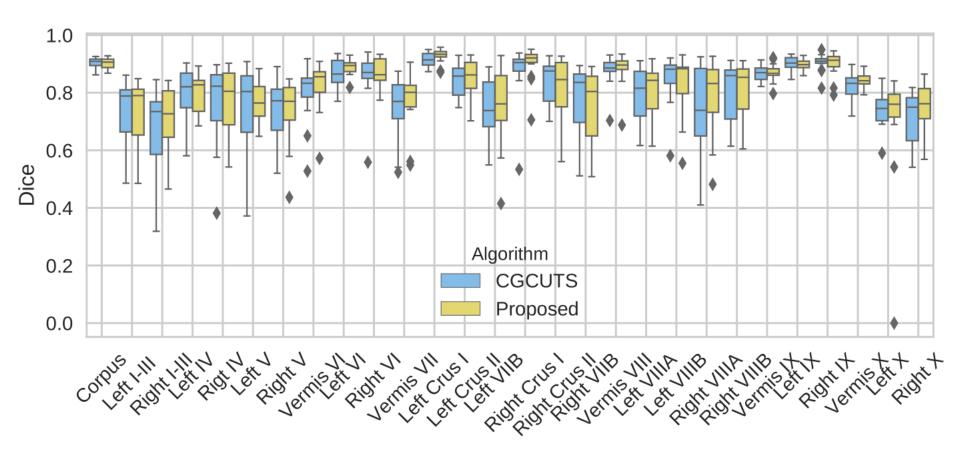
Segmenting Network



Example Results



Comparison to Leading Method



Deep Learning

OTHER NOTIONS AND METHODS

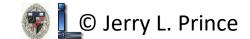


Problem with Deep Models

- A two-layer NN can approximate any continuous function
 - Why seek a deep network?
 - Ans: approximate complex functions to the same accuracy with fewer neurons/weights → train with a smaller training set
- Deep networks experience the "vanishing gradient problem"
 - Propagated errors "messages" get smaller and smaller due to repeated multiplications

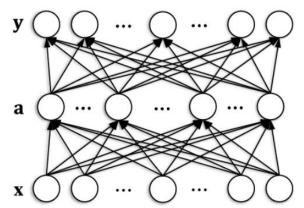
$$\frac{\partial E}{\partial \mathbf{W}^{(l)}} = \frac{\partial E}{\partial \mathbf{a}^{(L)}} \frac{\partial \mathbf{a}^{(L)}}{\partial \mathbf{a}^{(L-1)}} \cdots \frac{\partial \mathbf{a}^{(l+2)}}{\partial \mathbf{a}^{(l+1)}} \frac{\partial \mathbf{a}^{(l+1)}}{\partial \mathbf{a}^{(l)}} \frac{\partial \mathbf{a}^{(l)}}{\partial \mathbf{z}^{(l)}} \frac{\partial \mathbf{z}^{(l)}}{\partial \mathbf{W}^{(l)}}$$

- Solutions?
 - Alternative activation functions (e.g., hyperbolic tangent, soft sign)
 - Greedy layer-wise pretraining: pretrain using unsupervised approach each layer and then fine-tune the joint network



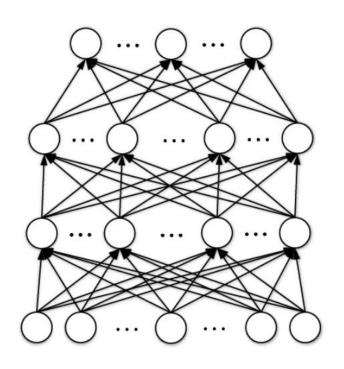
Auto-Encoder

- Unsupervised way to train a neural network to reconstruct itself!
- Basic idea is to encourage y to resemble x → no label data at all
- Use the loss function: $E(X,Y) = \frac{1}{2} \sum_{i=1}^{N} ||x_i y_i||^2$ # neurons in hidden layer can be smaller than # inputs
- - Dimensionality reduction
- # neurons in hidden layer can be larger than # inputs
 - Encourage sparseness
 - Discover hidden structure



Stacked-Auto Encoder

- Greatly improves the representational power
- Lower layers learn simple patterns in the image
- Higher layers learn abstract patterns/relationships
- Training
 - Initialize weights randomly
 - Use backpropagation
- Greedy training
 - Train lowest layer
 - Fix outputs; train next layer, and so on
- Classification task
 - Stack an output layer on top
 - Train it with SAE fixed
 - Fine tune entire network



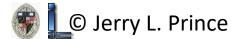


Restricted Boltzmann Machine

- Two layer, undirected graphical model
 - Visible layer with bias term
 - Hidden layer with bias term
 - Symmetric connectivity between layers; no connectivity within layers
- Symmetry of connections
 - Learn hidden layer from observations, and
 - Reconstruct observations from hidden layer
 - Therefore, RBM is a type of auto-encoder
- Joint probability between v and h

$$P(\boldsymbol{v}, \boldsymbol{h}, \Theta) = \frac{1}{Z(\Theta)} \exp[-E(\boldsymbol{v}, \boldsymbol{h}, \Theta)]$$

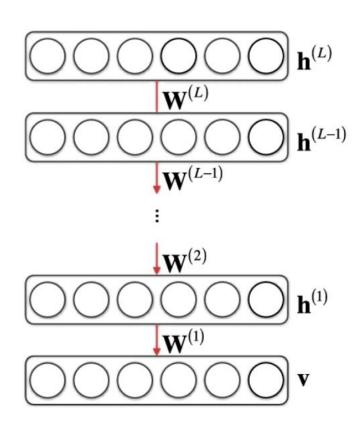
$$E(\mathbf{v}, \mathbf{h}, \Theta) = -\sum_{i=1}^{D} \sum_{j=1}^{F} v_i W_{ij} h_j - \sum_{i=1}^{D} a_i v_i - \sum_{j=1}^{F} b_j h_j$$

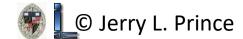


Hidden layer

Deep Belief Network

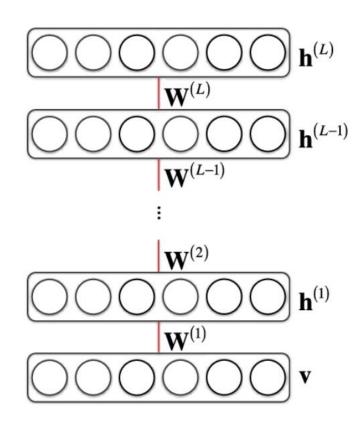
- Stack multiple hidden layers above a visible layer
 - Top two layers are bidirectional
 - Remaining layers are directed "generative" edges
- Remains an auto-encoder
- Greedy layer-wise training can be used
- Use trained weights in DBN for a deep neural network for classification

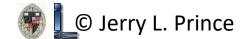




Deep Boltzmann Machine

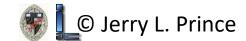
- Stack hidden layers on a visible layer
 - All layers are bidirectional
- Still thought of as autoencoder
- Training
 - Generative trains on minimization of negative log likelihood
 - Classification trains on minimization of negative posterior density





Deep Learning

RESOURCES



Software for Deep Networks

Table 2.1

A curated list of software for Convolutional Neural Networks

Software	Interfaces provided	AutoDiff
Caffe [53]	Python, MATLAB, C++, command-line	No
Theano [91]	Python	Yes
Tensorflow [5]	C++, Python	Yes
Torch [4]	Torch, C	Yes (non-native)
CNTK [6]	C++, command-line	No
MatConvNet [94]	MATLAB	No
Chainer [1]	Python	No

Data for Training

https://grand-challenge.org

Contributors

The authors of this site are <u>Bram van Ginneken</u>, <u>Sjoerd Kerkstra</u>, and <u>James Meakin</u>.

Grand Challenges in Biomedical Image Analysis								
All Challenges								
Here is an overview of all challenges that have been organized within the area of medical image analysis that we are aware of. If you know any study that would fit in this overview, please leave a message in the <u>forum</u> .								
Showing 143 projects of 143								
Filter by:	Data download (94)	Hosted on Grand-challenge (17)						
2017								
Workshop: Sep 10, 2017 Associated with: MICCAI 2017 Hosted on: grand-challenge.org	Associated with: ISBI 2017 Hosted on: grand-challenge.org	Data download Workshop: Sep 14, 2017 Associated with: MICCAI 2017 Hosted on: grand-challenge.org						
EndoVis	CAMELYON17	RETOUCH						
As an endoscopic vision CAI challenge at MICCAI, our aim is to provide a formal framework for evaluating the current state of the art, gather researchers in the field and provide high quality data with protocols for validating endoscopic vision algorithms.	Automated detection and classification of breast cancer metastases in whole-slide images of histological lymph node sections. This task has high clinical relevance and would normally require extensive microscopic assessment by pathologists.	The goal of the Retinal OCT Fluid Challenge is to compare automated algorithms that are able to detect and segment various types of retinal fluid lesions on a common dataset of optical coherence tomography (OCT) volumes representing different retinal diseases, acquired with devices from different manufacturers.						
Open for submissions Data download Hosted on: grand-challenge.org	Workshop: Aug 01, 2017 Associated with: <u>AAPM 2017</u> Hosted on: <u>grand-challenge.org</u>	Associated with: MICCAI 2017						

